





# Sub-Nyquist TEM-Based Hardware for Heart Rate Monitoring of ECG Signals

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# **Motivation and Contributions**

- Critical ADC tasks: Sampling and quantization play vital roles in an ADC
- Inefficient conventional ADCs: Conventional ADCs waste power and bandwidth due to underutilization of signal information
- ☐ TEM for signal encoding: Time encoding machines (TEM) encode input signals into time sequences, effectively utilizing signal information
- ☐ Enhanced noise robustness: Moving the quantization process from the signal amplitude domain to the time domain improves amplitude noise robustness
- □ Power-efficient sub-Nyquist sampling: Our presented TEM hardware enables efficient sub-Nyquist sampling and recovery of ECG signals, facilitating heart rate monitoring applications

# **ECG Sampling and Reconstruction**

- □ Variable width pulses:  $x(t) = \sum_{k=0}^{\infty} x_k(t)$ , where,  $x_k(t) = x_k^s(t) + x_k^a(t)$
- $\Box$  The signal components  $x_k^s(t)$ ,  $x_k^a(t)$  are the symmetric and antisymmetric parts of the pulse
- $\Box$  4L + 1 Fourier samples of x(t) uniquely determine the parameters  $\{t_k, r_k, c_k, d_k\}_{k=0}^{L-1}$
- $\Box$  If the signal is defined on the interval [0,T] the local the rate of innovation is  $\frac{4L+1}{T}$
- ☐ Sub-Nyquist sampling scheme enables computation of the Fourier samples from low rate samples

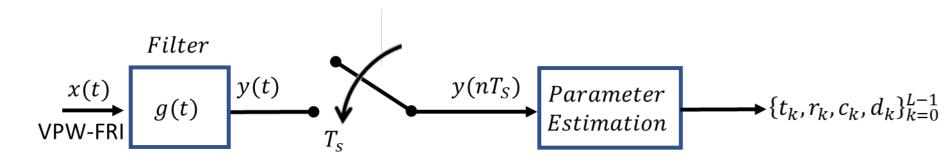


Fig: Sampling and reconstruction of VPW-FRI signal by using a sampling kernel g(t)

Baechler, G., Scholefield, A., Baboulaz, L., & Vetterli, M., 2017

 $C = \int_0^B \log_2\left(1 + \frac{S(f)}{N(f)}\right) df$ 

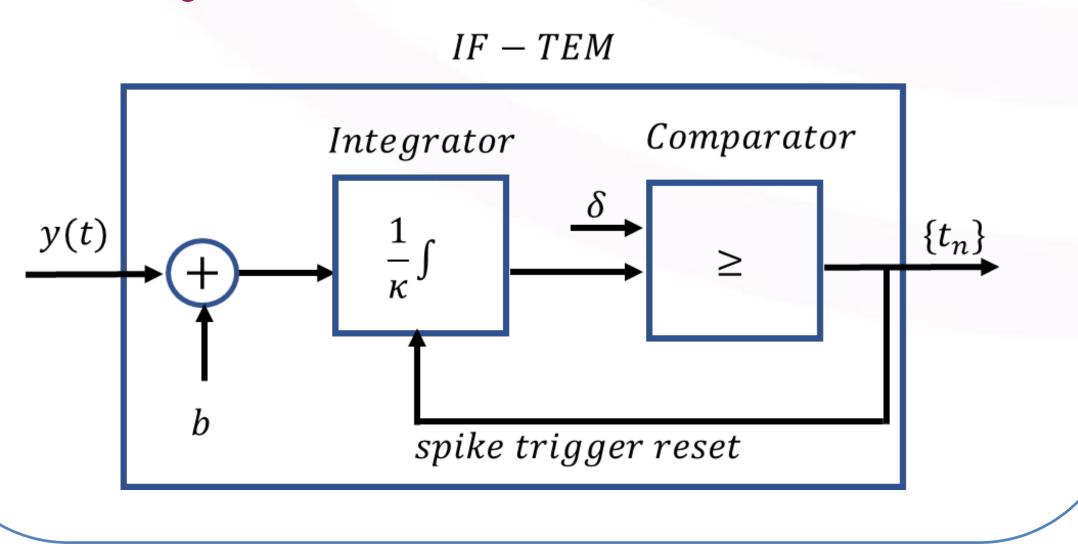
 $x_k^{S}(t) = c_k \sum_{p \in \mathbb{Z}} \frac{r_k}{\pi (r_k^2 + (t - t_k - pT)^2)}$  $x_k^{a}(t) = d_k \sum_{p \in \mathbb{Z}} \frac{t - t_k - pT}{\pi (r_k^2 + (t - t_k - pT)^2)}$ 

# IF-TEM

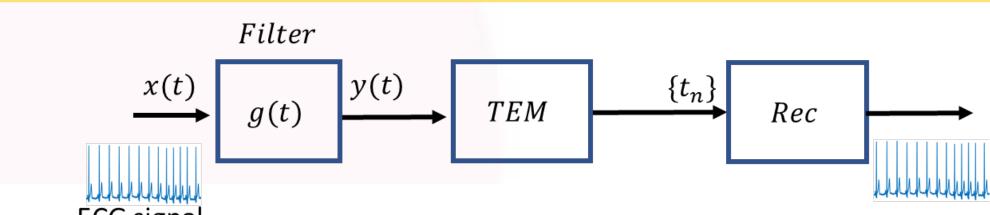
- ☐ An integrate-and-fire time-encoding machine is paramerised by:
- b: The bias

 $\delta$ : The threshold

 $\kappa$ : The integrator constant

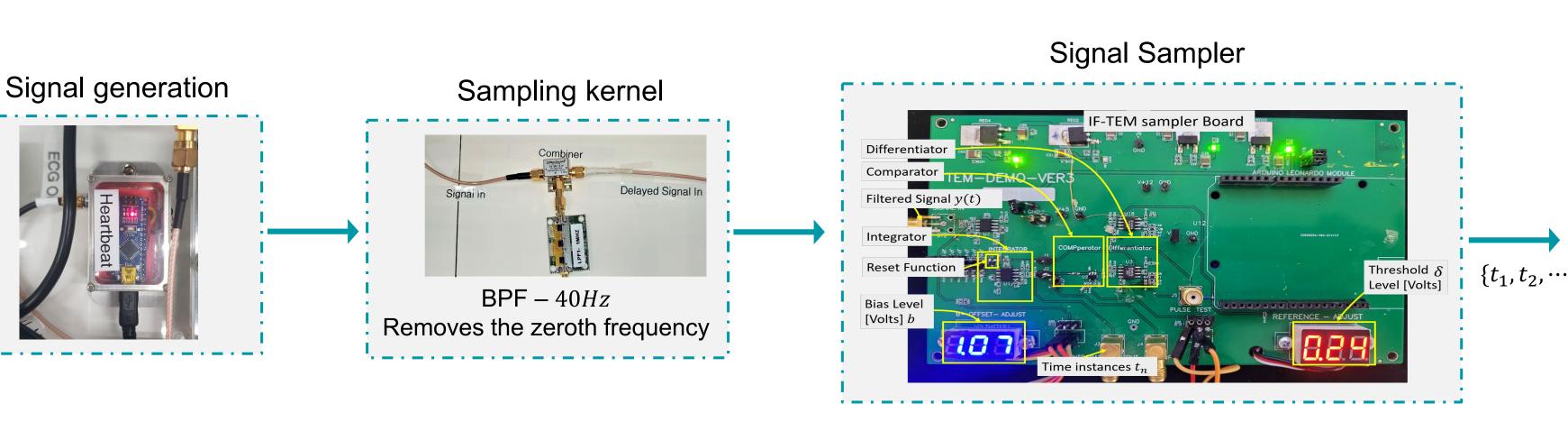


# **ECG-TEM Sampling**



- $\Box$  ECG signal modeling: We adopt a VPW-FRI signal model for the ECG signal within the interval [0, T]
- ☐ IF-TEM input and output: The IF-TEM takes in a filtered ECG signal and produces time instants as outputs
- $\Box$  Selection of IF-TEM parameters: We choose IF-TEM parameters to ensure there are 8L+2 time instants within the time interval T
- □ Definition of IF-TEM firing rate: The firing rate of the IF-TEM is determined by the number of time instants in the interval [0,T]
- □ Computation of Fourier coefficients and estimation: By utilizing TEM time instants, we compute the Fourier coefficients of / x(t) and estimate VPW-FRI parameters from them

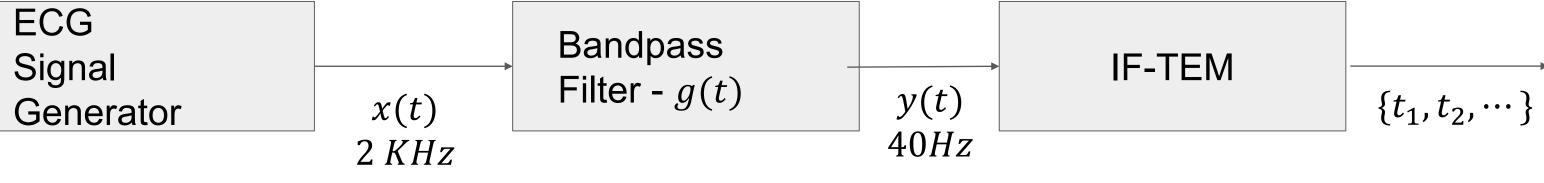
#### Hardware



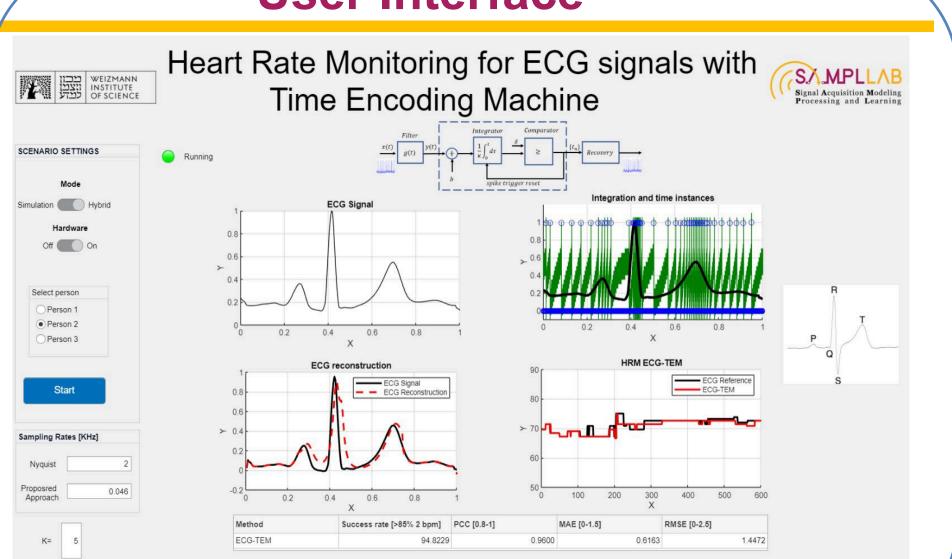
DSP

Reconstructed **ECG** 

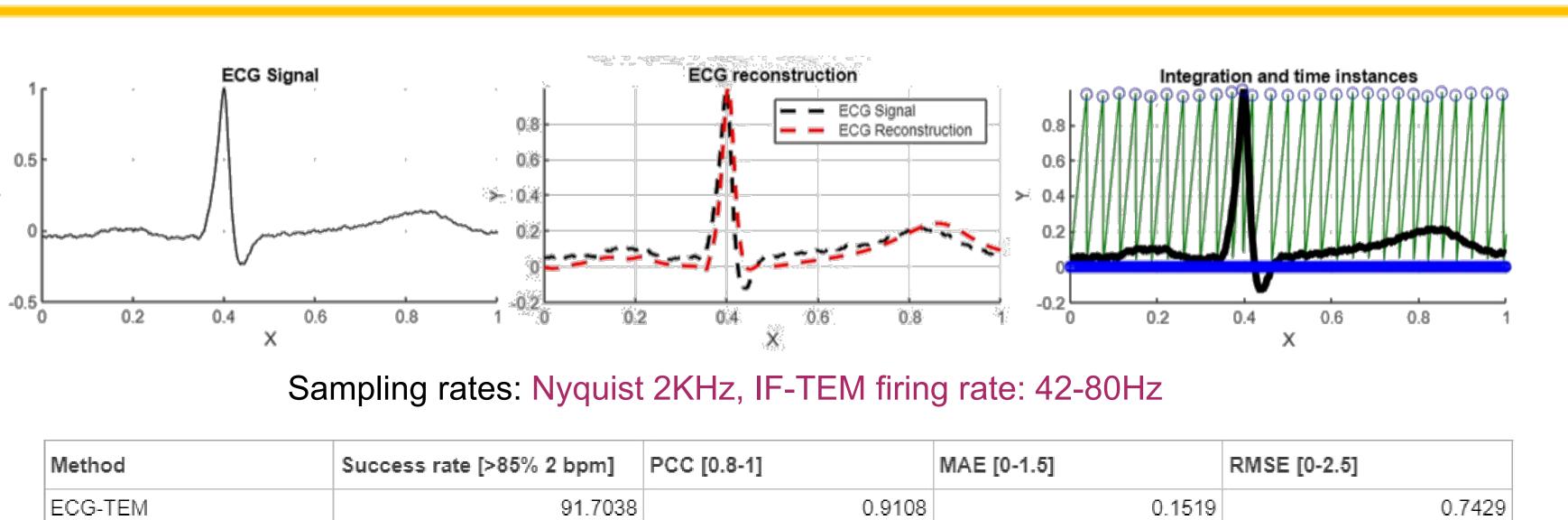
Reconstruction



### **User Interface**



# Results – ECG reconstruction and HRM



200 300 400 500 600 70

- ☐ The HRM is calculated from the recovered ECG signal
- ☐ Specifically, we examined the resting scenario, and compared the statistical metrics of the HR estimate with the reference output

#### Conclusions

- ☐ Power-efficient sub-Nyquist sampling: Our TEM hardware enables efficient sub-Nyquist sampling and recovery of ECG signals, benefiting heart rate monitoring
- ☐ Enhanced noise robustness: The ECG signal is filtered to remove its zeroth frequency to improve noise resilience
- ☐ The processed filtered signal, y(t), is sampled using an IF-TEM sampler, resulting in a firing rate of 42-80Hz, equivalent to approximately 1/20-1/40 of the Nyquist rate

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