

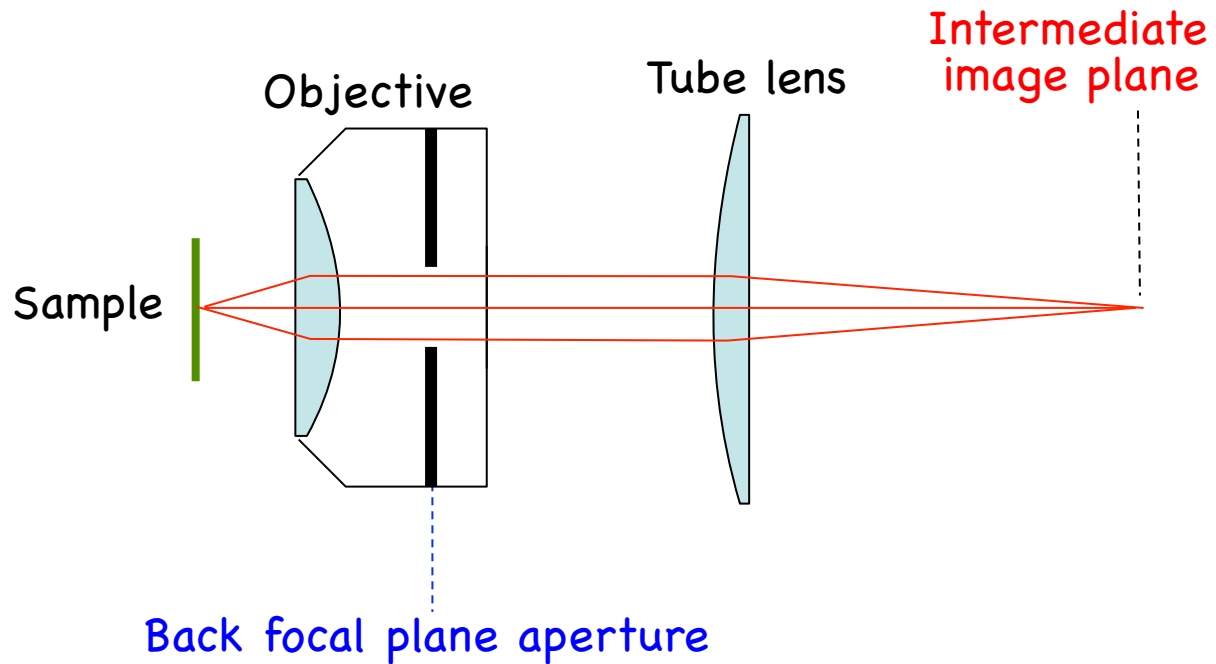
Principles & Practice of Light Microscopy 2

- Resolution
- Aberrations
- The Point Spread Function
- The Optical Transfer Function
- Spatial frequencies

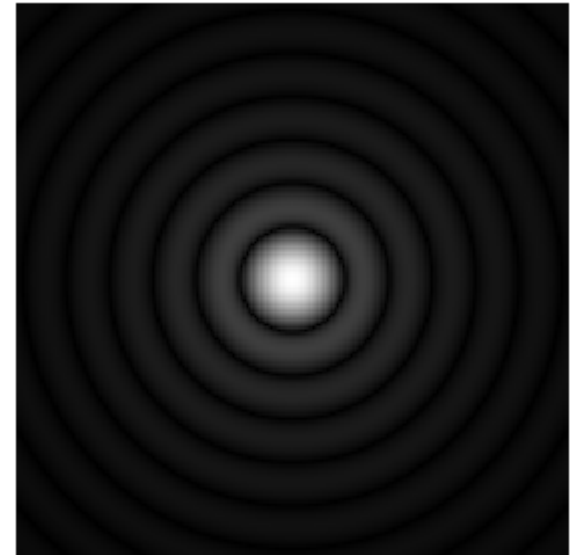
Edited by: Zvi Kam, Weizmann
For Advance Light Microscopy course

RESOLUTION

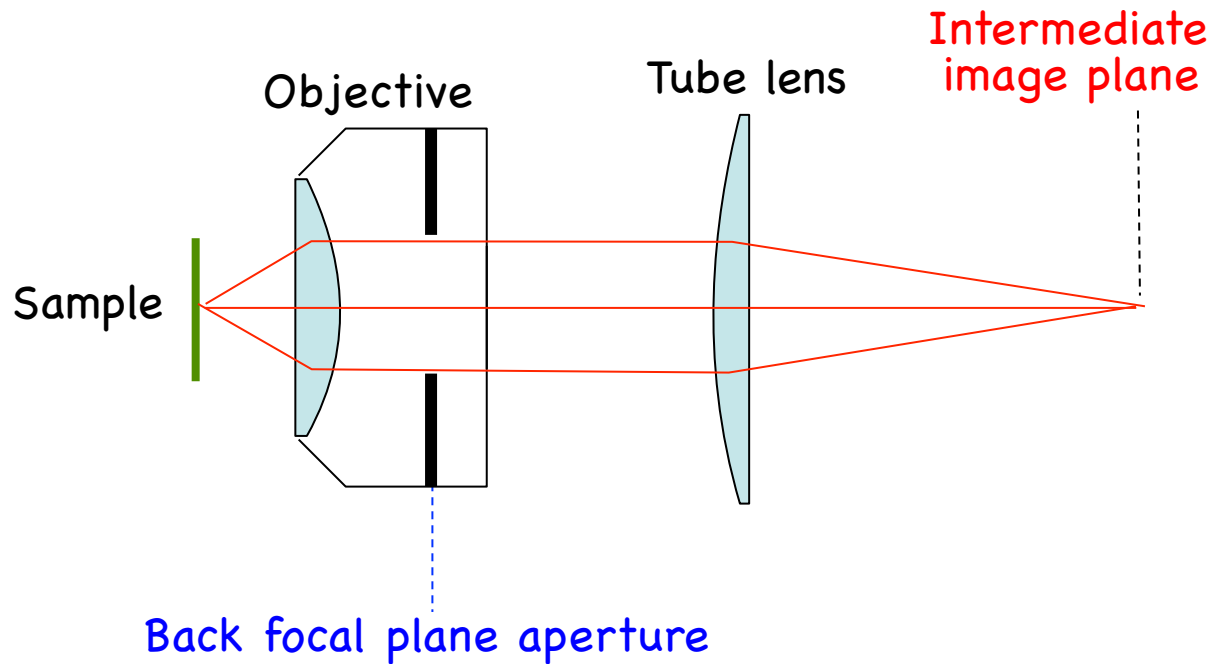
Aperture and Resolution



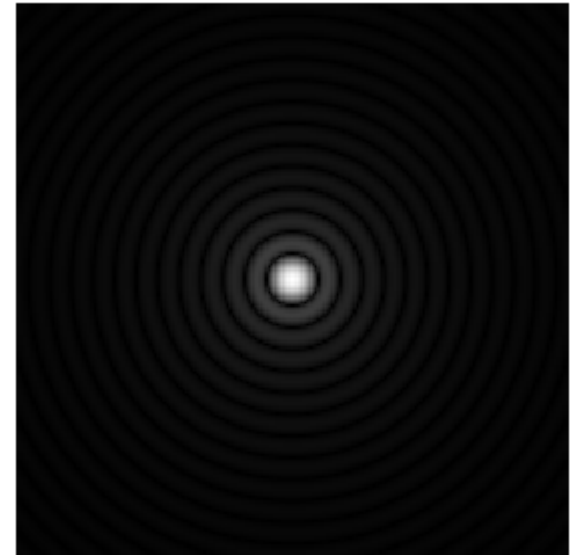
Diffraction spot
on image plane
= *Point Spread Function*



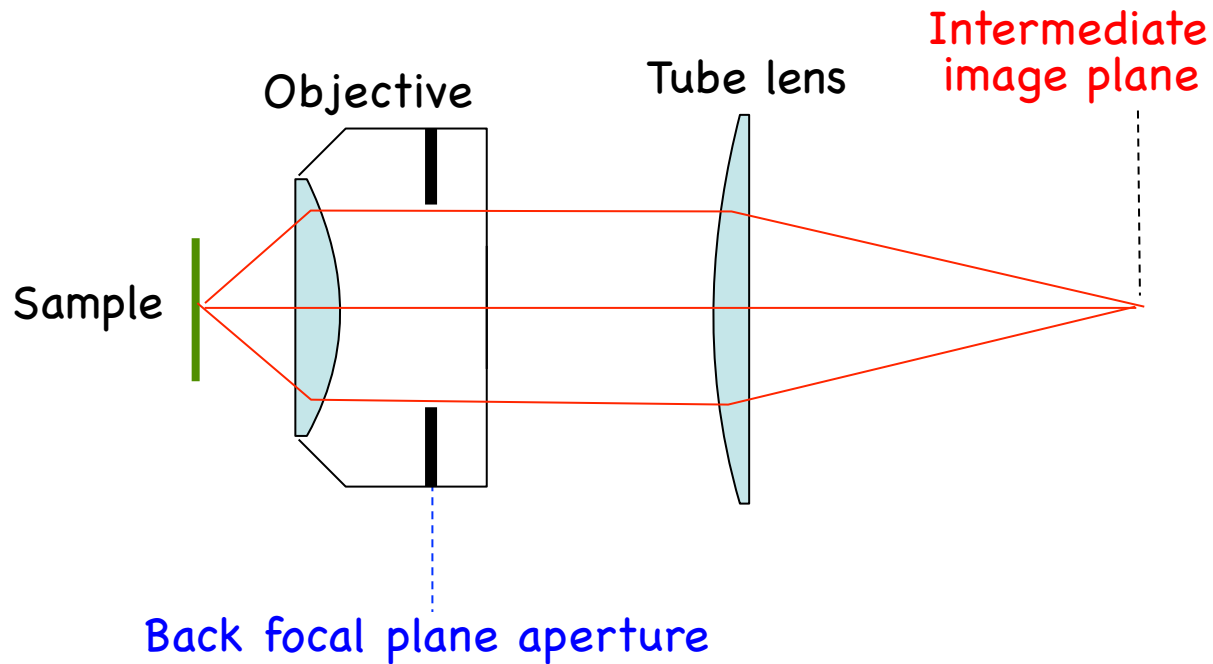
Aperture and Resolution



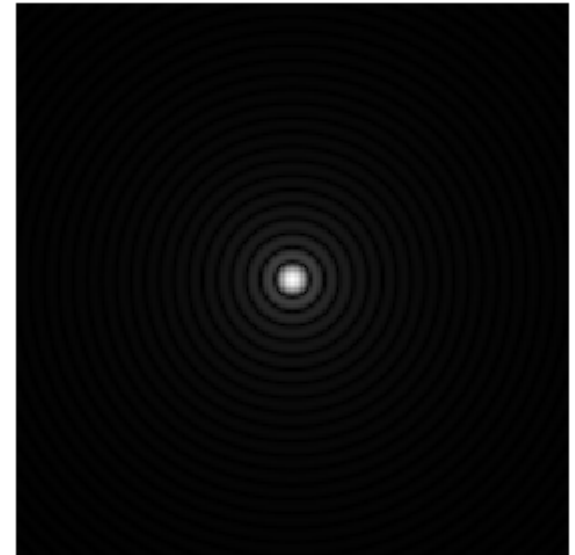
Diffraction spot
on image plane
= *Point Spread Function*



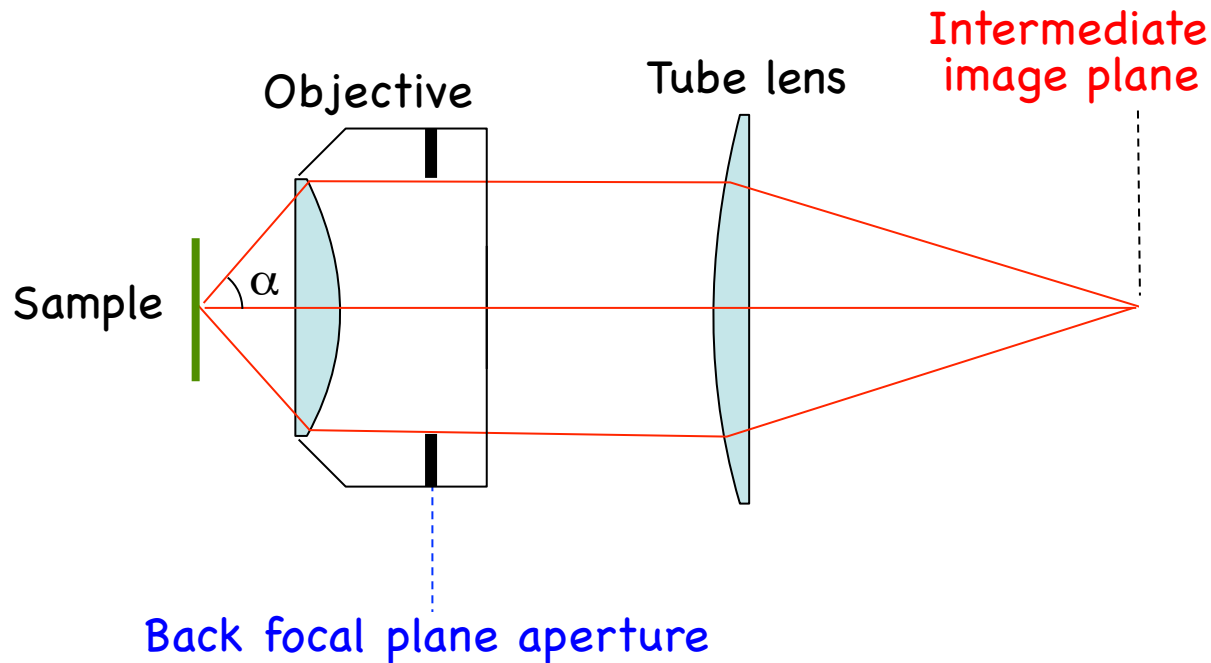
Aperture and Resolution



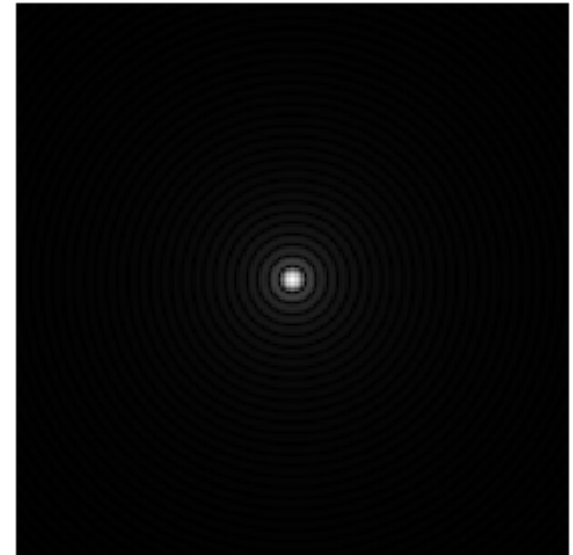
Diffraction spot
on image plane
= *Point Spread Function*



Aperture and Resolution



Diffraction spot
on image plane
= *Point Spread Function*



- Image resolution improves with Numerical Aperture (NA)

$$NA = n \sin(\alpha)$$

where:

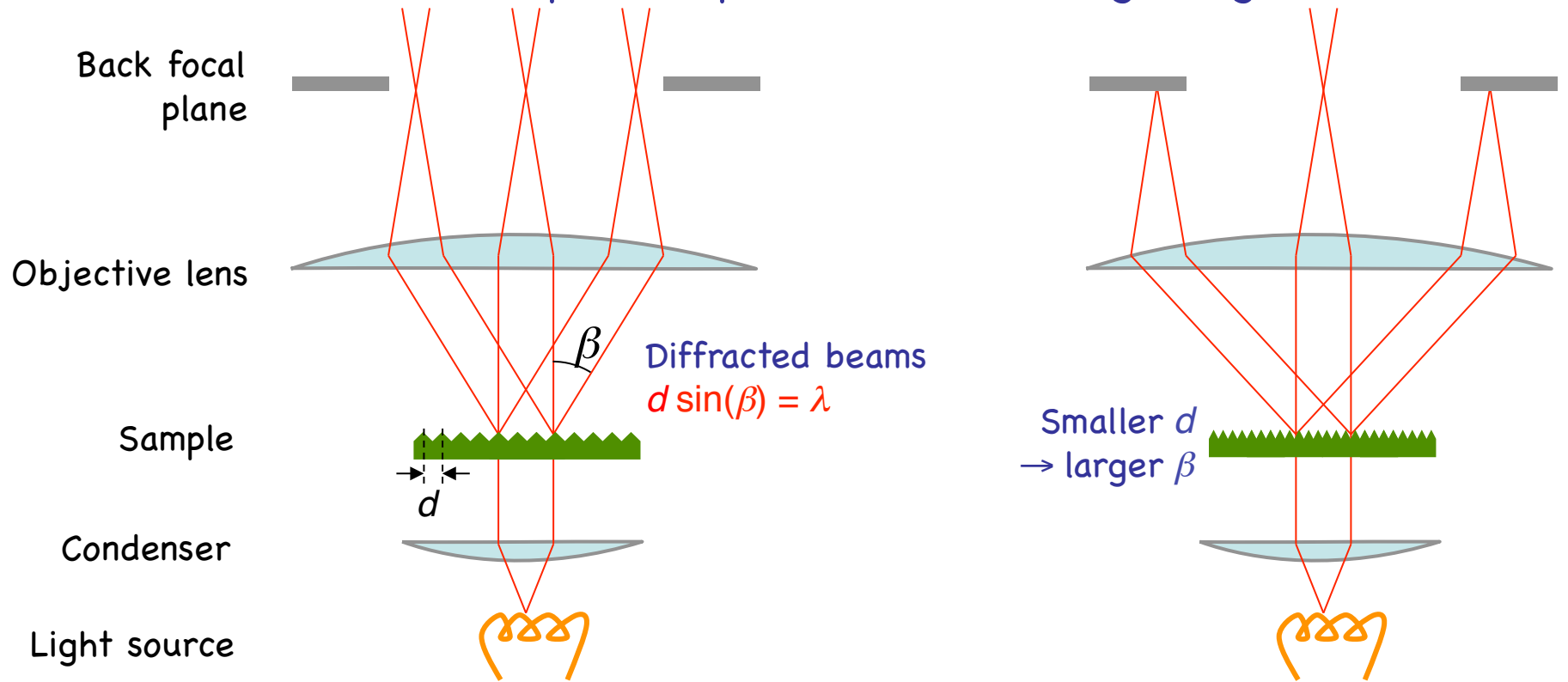
α = light gathering angle

n = refractive index of sample

Resolution

Ernst Abbe's argument (1873)

Consider a striped sample \approx a diffraction grating



Consider first
a point light source

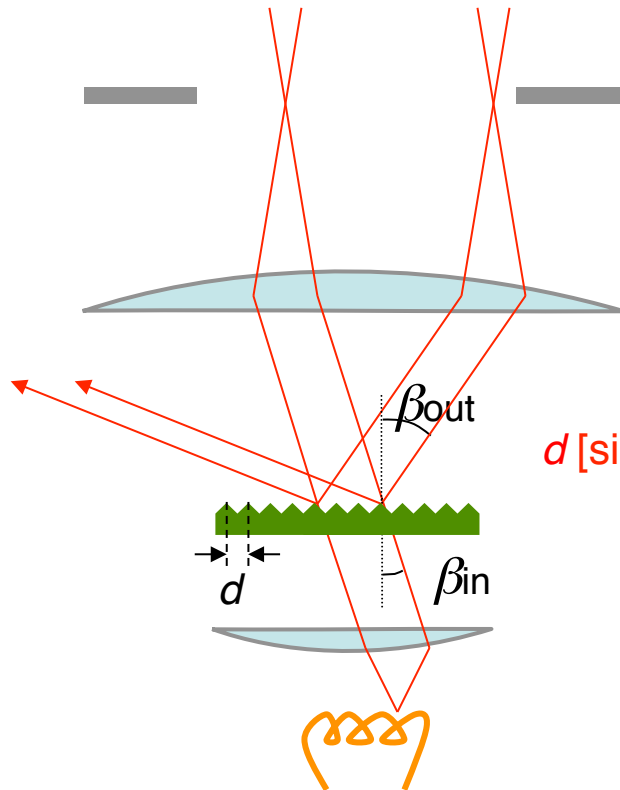
If $\beta > \alpha$, only one spot makes it through
 \Rightarrow no interference \Rightarrow no image formed

Resolution (smallest resolvable d):

$$d_{\min} = \lambda_{\text{sample}} / \sin(\alpha) = \lambda / n \sin(\alpha) = \lambda / NA$$

(Abbe's argument, continued)

Now consider oblique illumination
(an off-axis source point):



One spot hopelessly lost,
but **two** spots get through
→ interference → image formed!

$$d [\sin(\beta_{in}) + \sin(\beta_{out})] = \lambda$$

Two spots get through if
 $\beta_{out} < \alpha$ and $\beta_{in} < \alpha$.

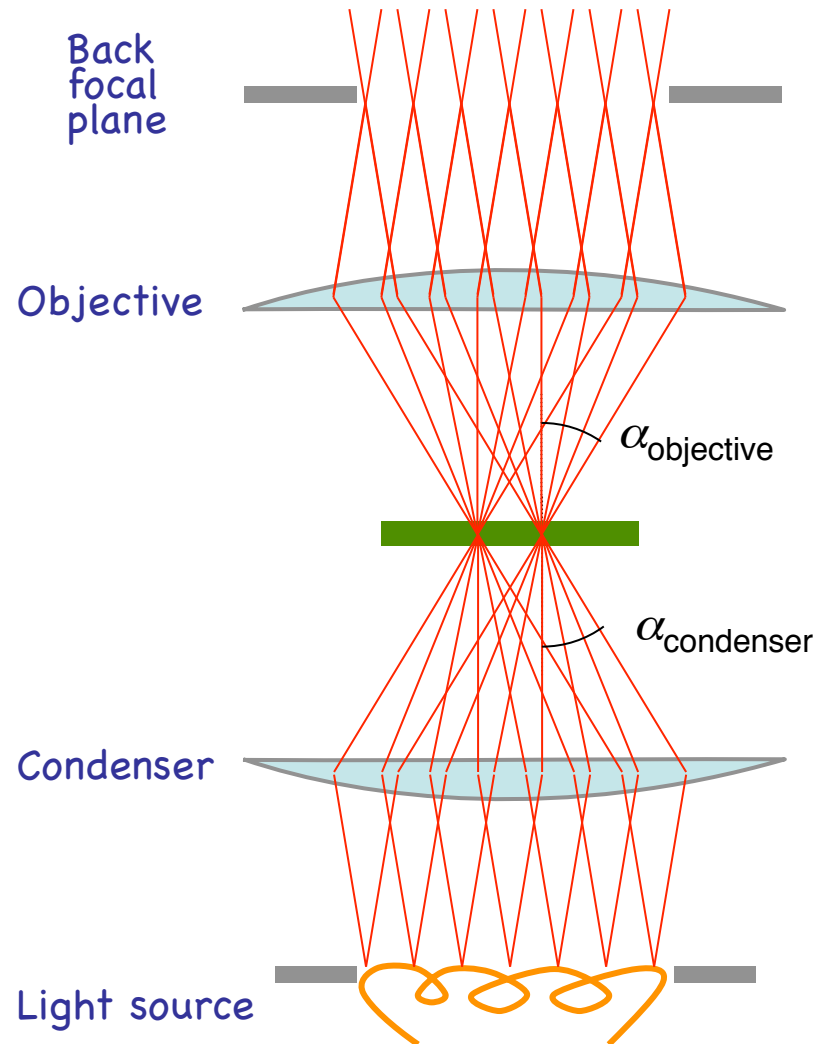
Resolution (smallest resolvable d)
with incoherent illumination (all possible illumination directions):

$$d_{min} = \lambda / (NA_{obj} + NA_{condenser})$$

→ $\lambda/2 NA$ if $NA_{condenser} \geq NA_{obj}$ (“Filling the back focal plane”)

Filling the back focal plane

In trans-illumination microscopy, to get maximum resolution, the illumination must “fill the back focal plane”



For the highest resolution, we need to have

$$\alpha_{\text{condenser}} \geq \alpha_{\text{objective}}$$

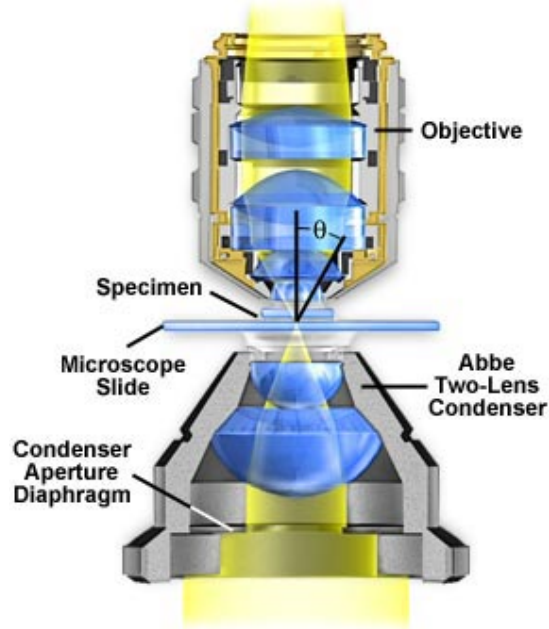


$$NA_{\text{condenser}} \geq NA_{\text{objective}}$$

\Rightarrow with oil immersion objectives, we need an *oil immersion condenser!*

The Condenser

Abbe Condenser Optical Pathway



Tasks:

- Illuminate at all angles $< \alpha_{\text{objective}}$
- Concentrate light on the field of view for *all* objectives to be used

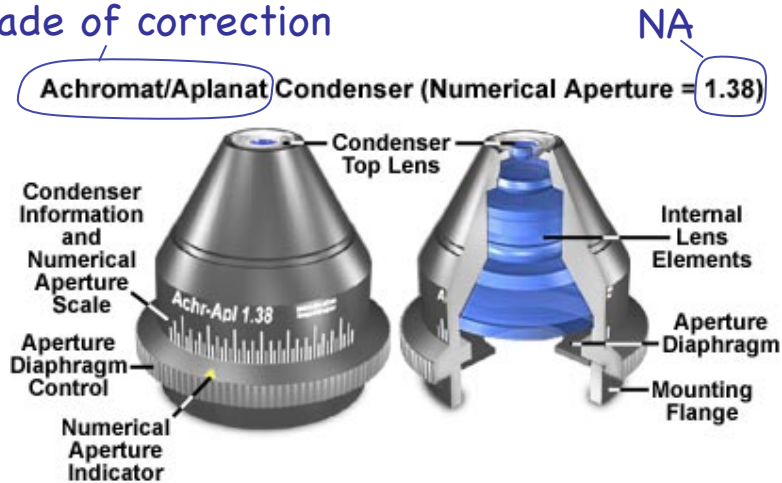
Problem:

- Low mag objectives have large FOV,
- High mag objectives have large α
(With 2X and 100x objectives we need $(100/2)^2 = 2500$ times more light than any objective uses!)

Solutions:

- Compromise
- Exchangable condensers, swing-out front lenses,...

Grade of correction

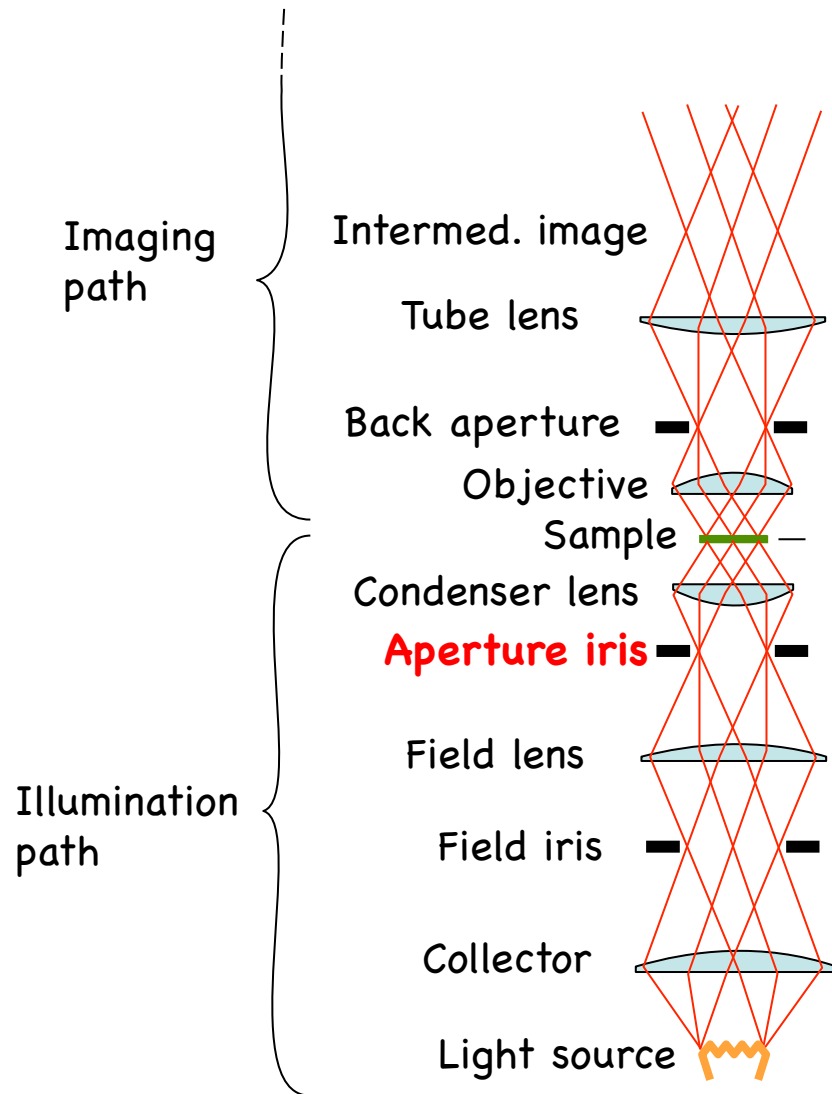


Swing-Out Top Lens Condenser (Numerical Aperture = 1.35)



Aperture, Resolution & Contrast

Can adjust the condenser NA with the **aperture iris**

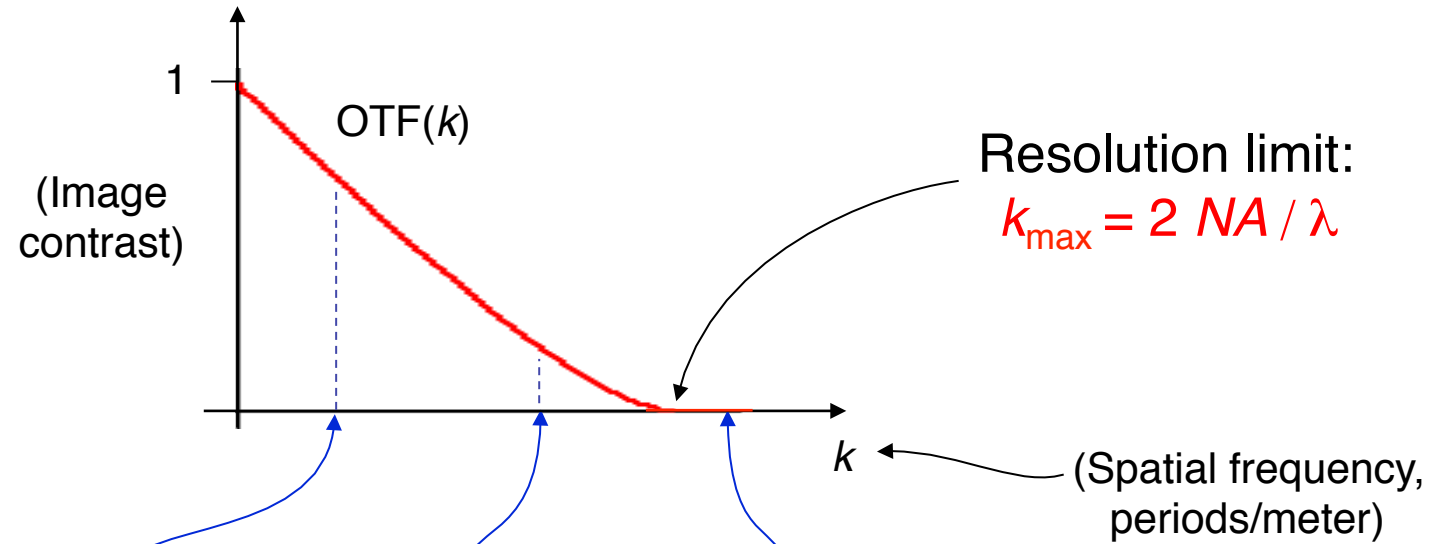


Q: Don't we always want it full open??

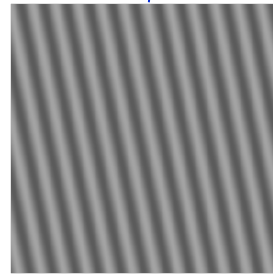
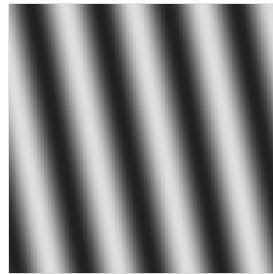
A: No

Why? Tradeoff:
resolution vs. **contrast**

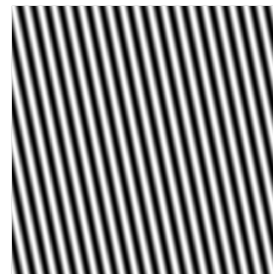
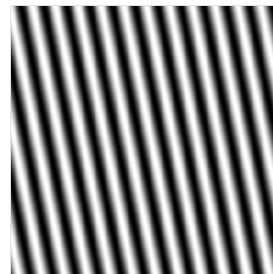
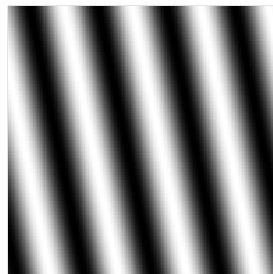
Spatial frequencies & the Optical Transfer Function (OTF)



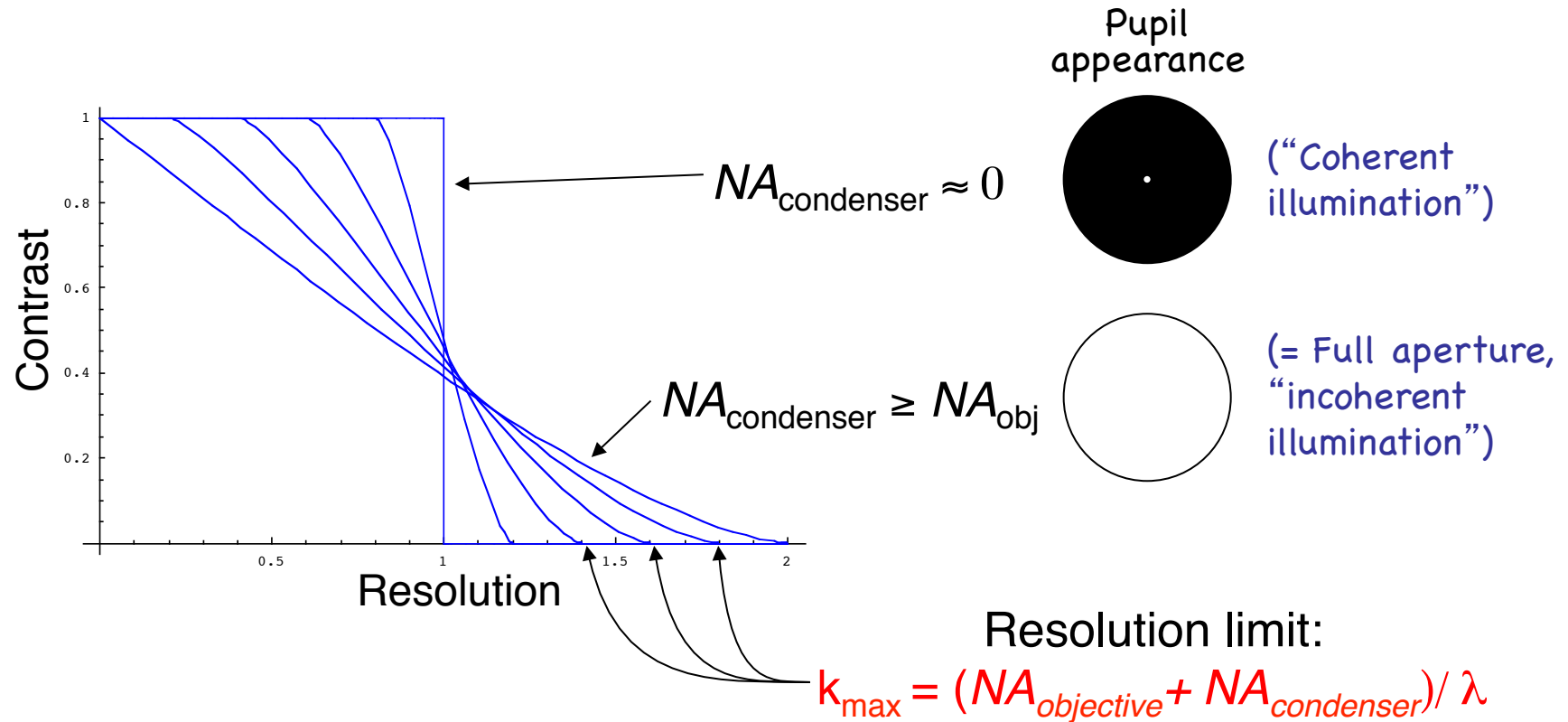
Observed image



Object



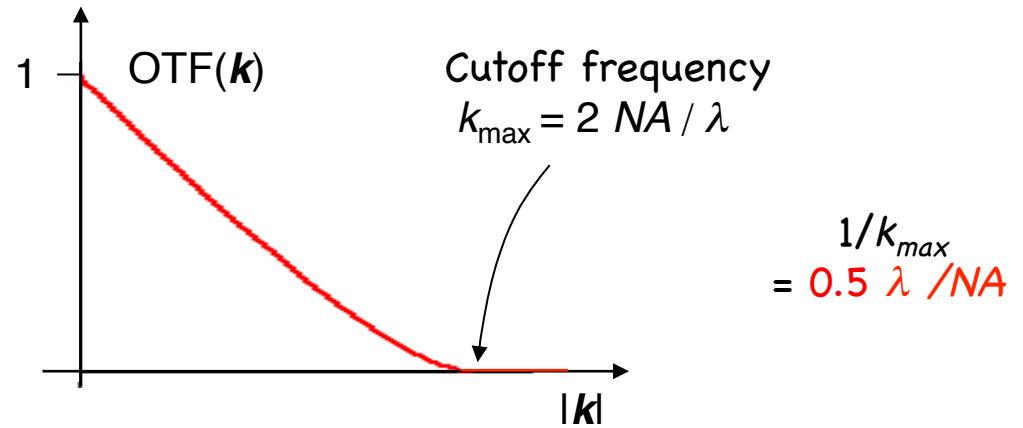
Resolution & Contrast vs. Illumination aperture



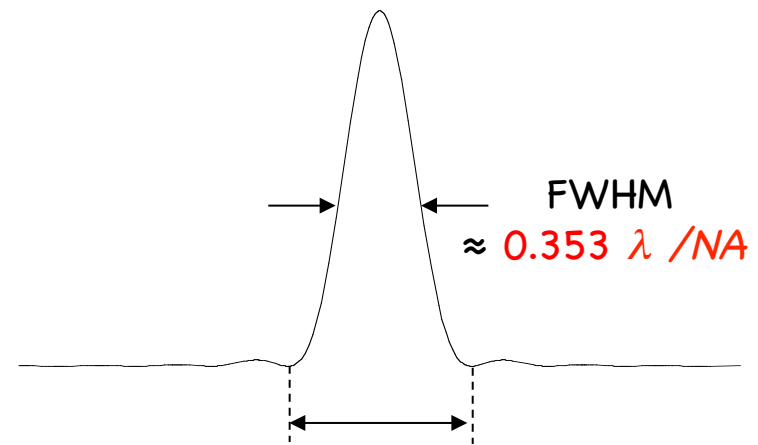
Increasing the illumination aperture
increases resolution
but decreases contrast

Definitions of Resolution

As the OTF cutoff frequency



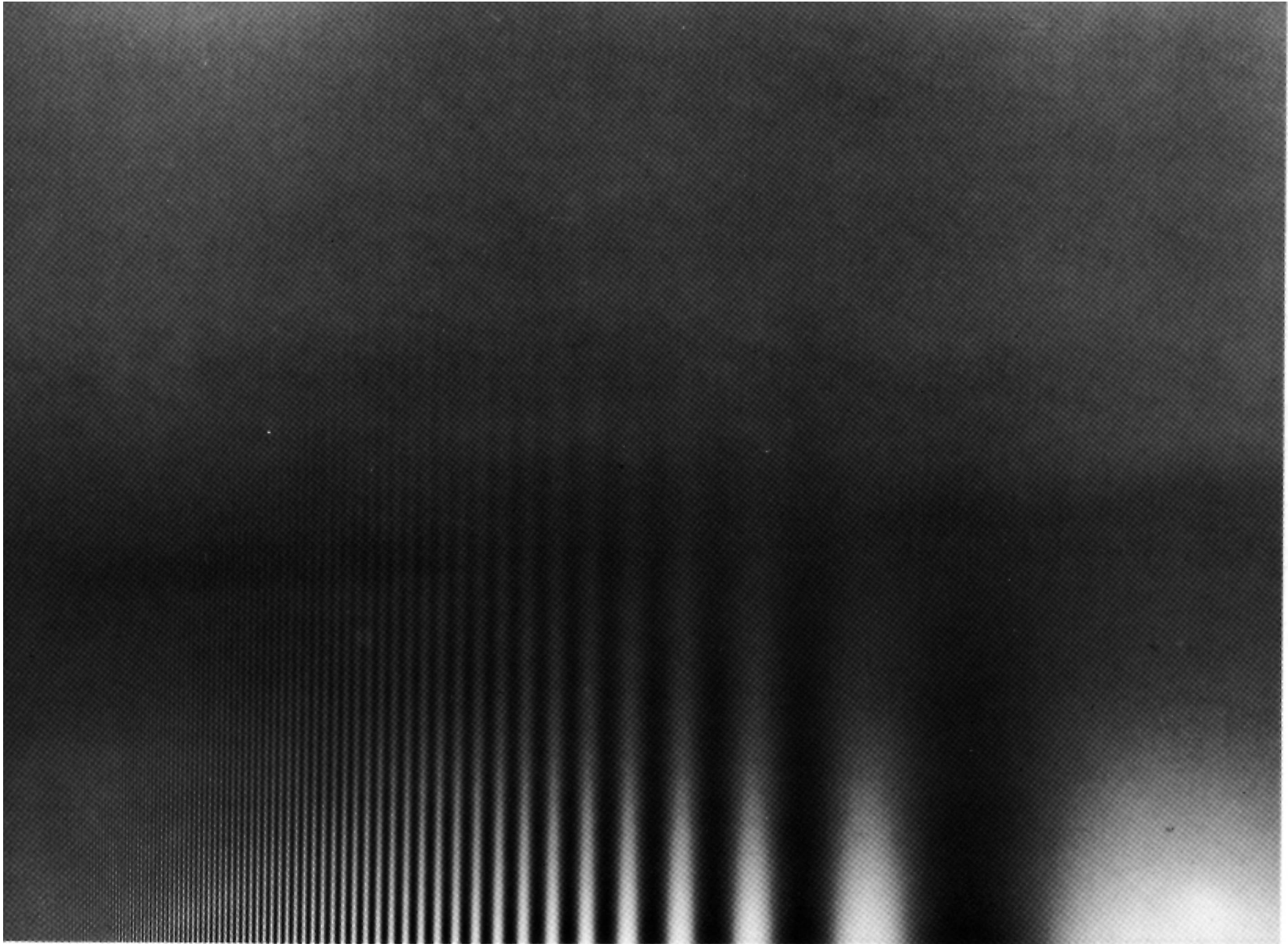
As the Full Width at Half Max (FWHM) of the PSF

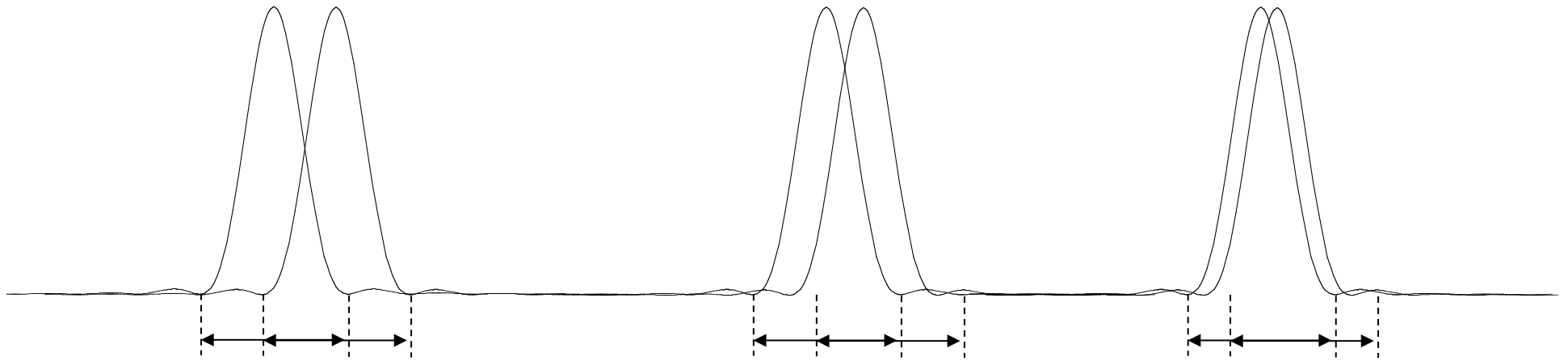


As the diameter of the Airy disk (first dark ring of the PSF) = "Rayleigh criterion"

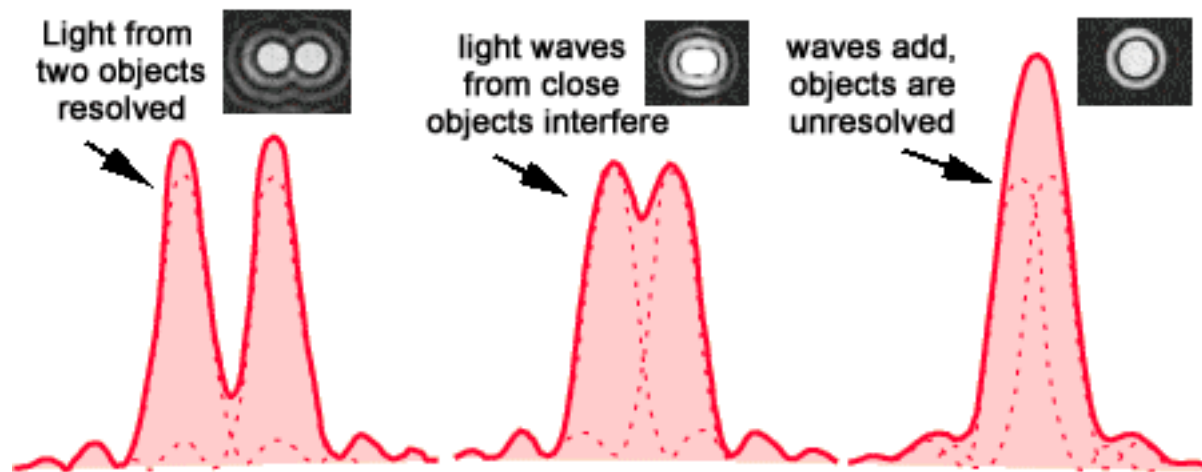
Airy disk diameter $\approx 0.61 \lambda / NA$

Contrast-resolution link





Rayleigh criterion: zero background



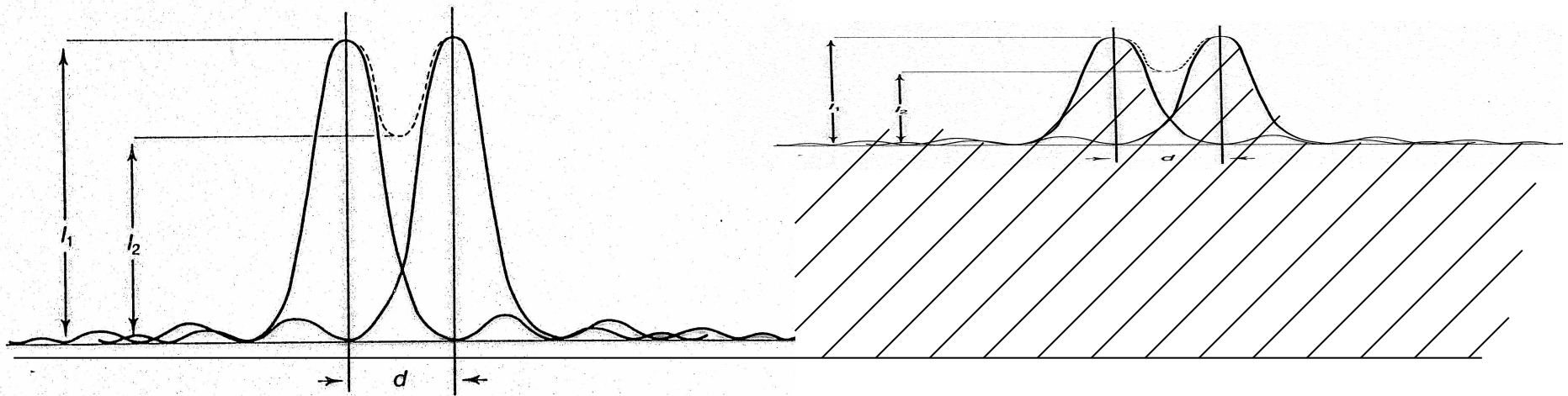
$I_2 / I_1 \sim 70\%$

$d = 0.61\lambda / NA$

$NA = 1.4 \quad d = 0.22 \mu m$

What is the complex optics for?

**The practice of microscopy,
or:
The fight for contrast.**



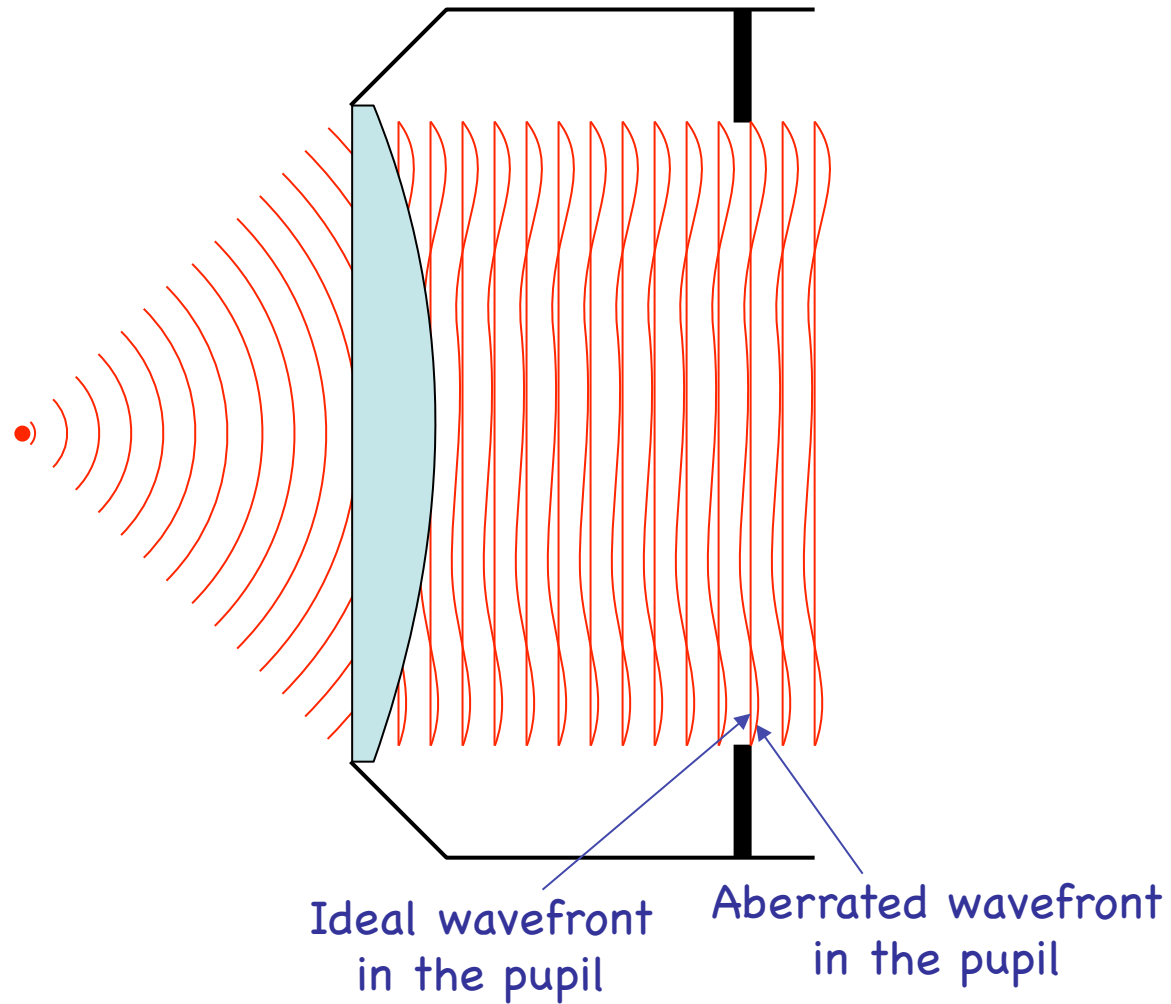
Aberrations

They are the enemy

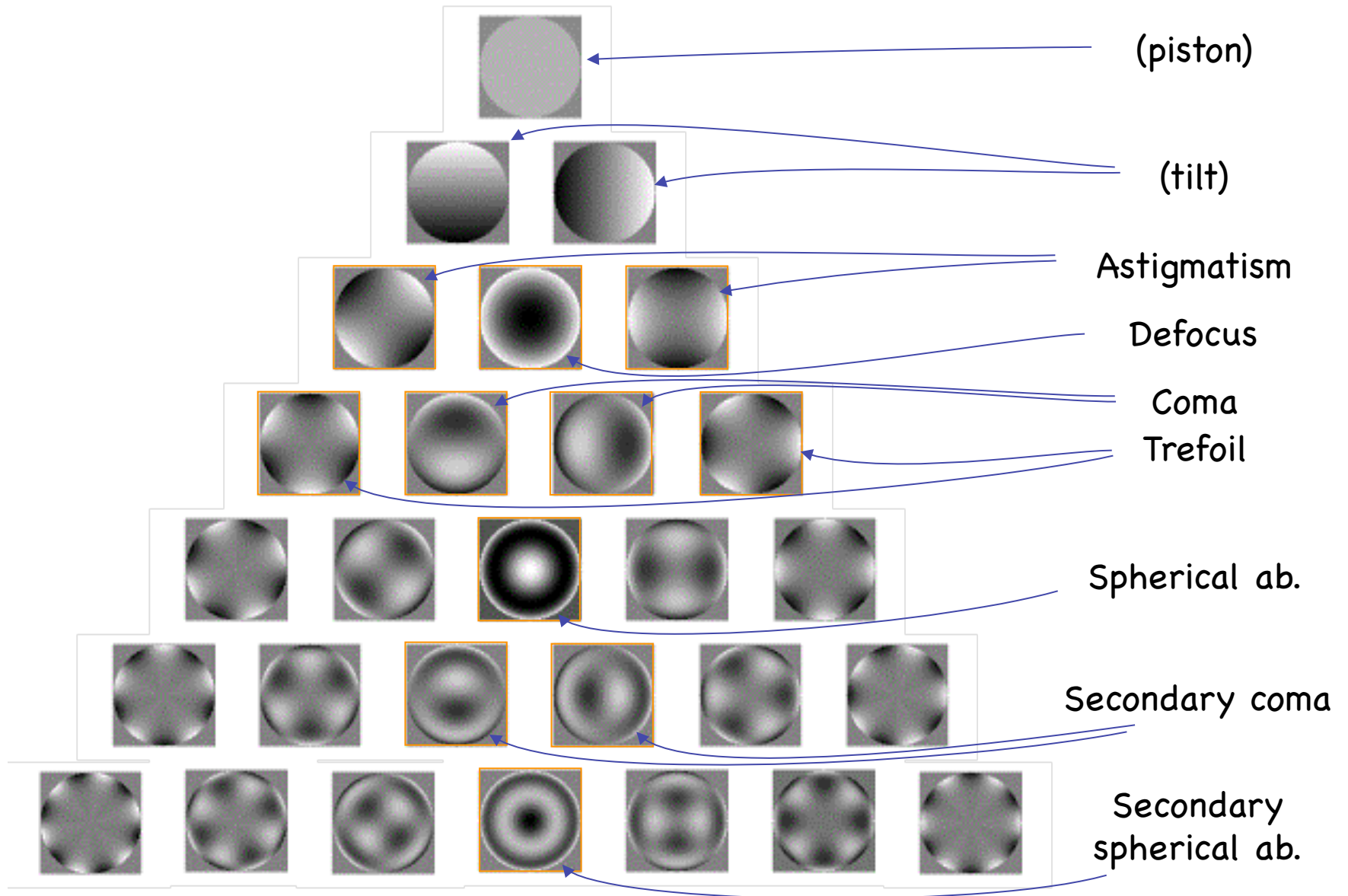
Aberrations: wave description

- Chromatic aberrations
 - Longitudinal chr. Ab.
 - Lateral chr. Ab.
- Curvature of field
- Distortion
- Wavefront aberrations
 - Spherical aberration
 - Astigmatism
 - Coma
 - ...

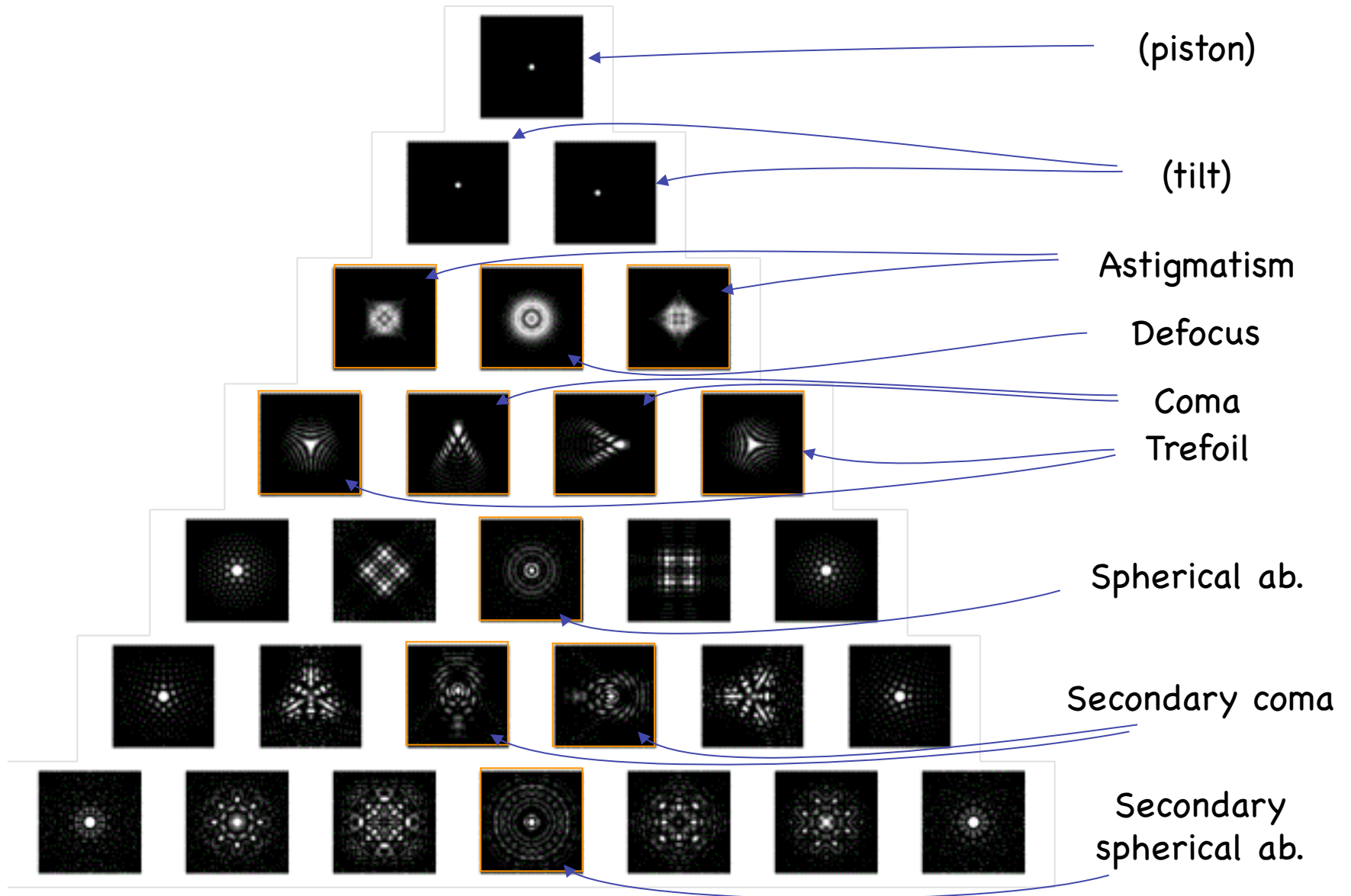
Wavefront Aberrations



Wavefront Aberrations



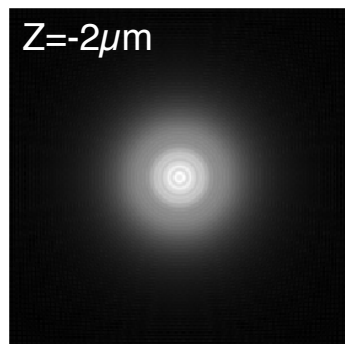
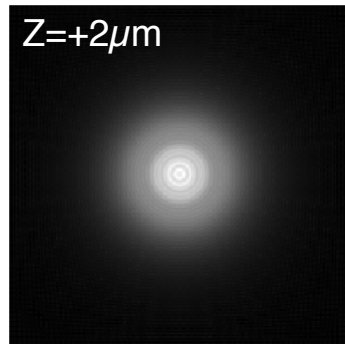
PSF Aberrations



The 3D Point Spread Function (PSF)

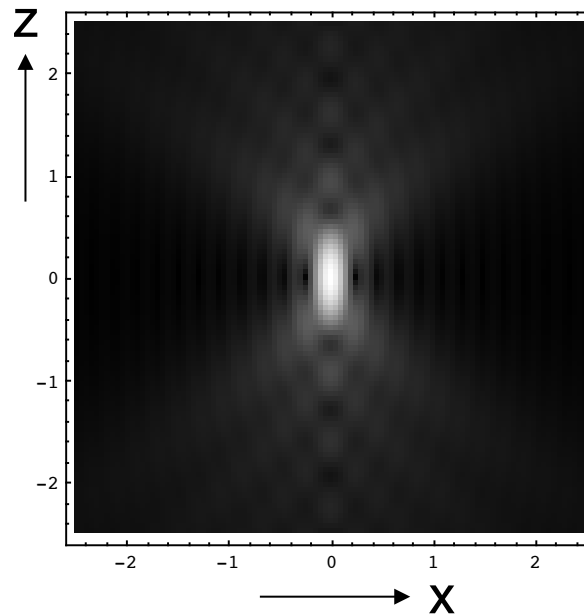
The image of a point object

2D PSF
for different defocus

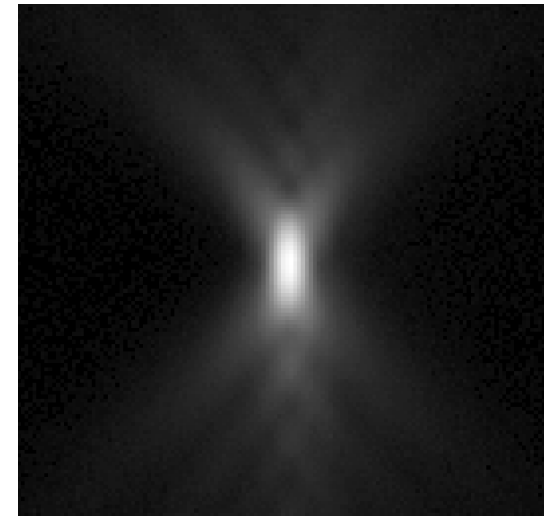


3D PSF

Calculated

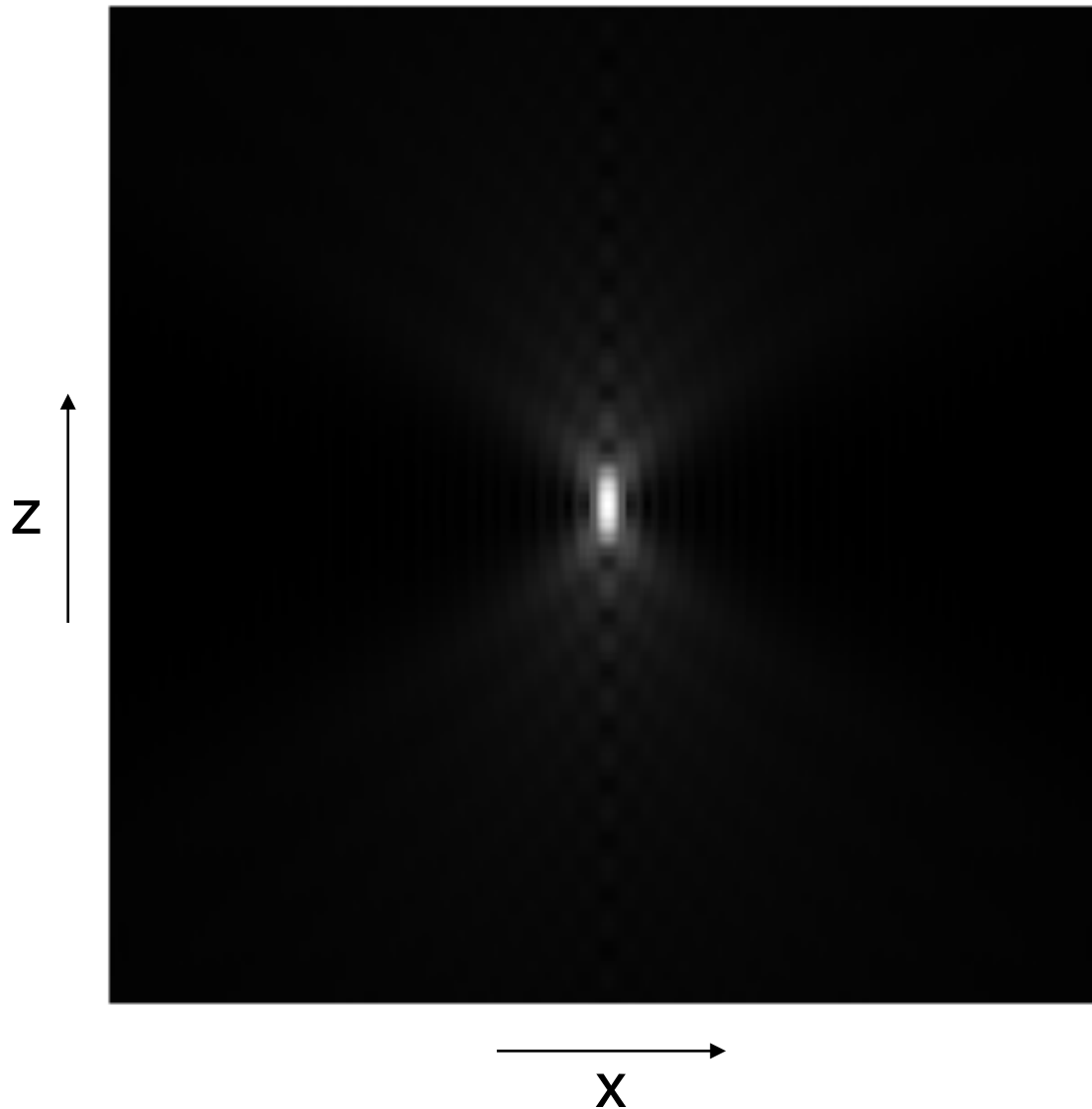


Measured



Spherical Aberration

Point spread function

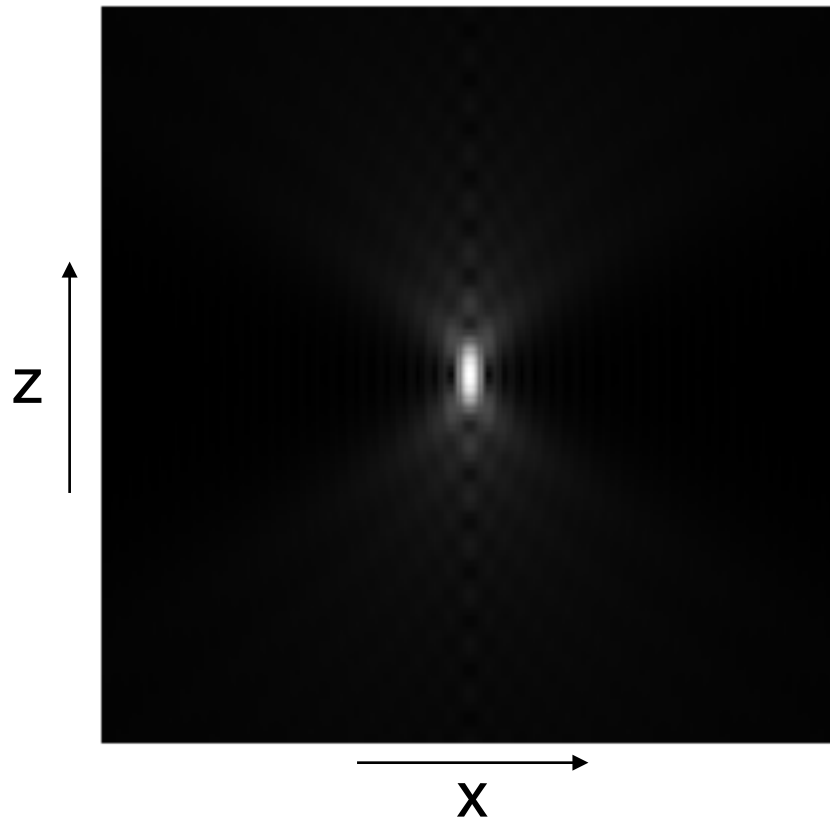


0-1 wave p-p
of primary
spherical ab.

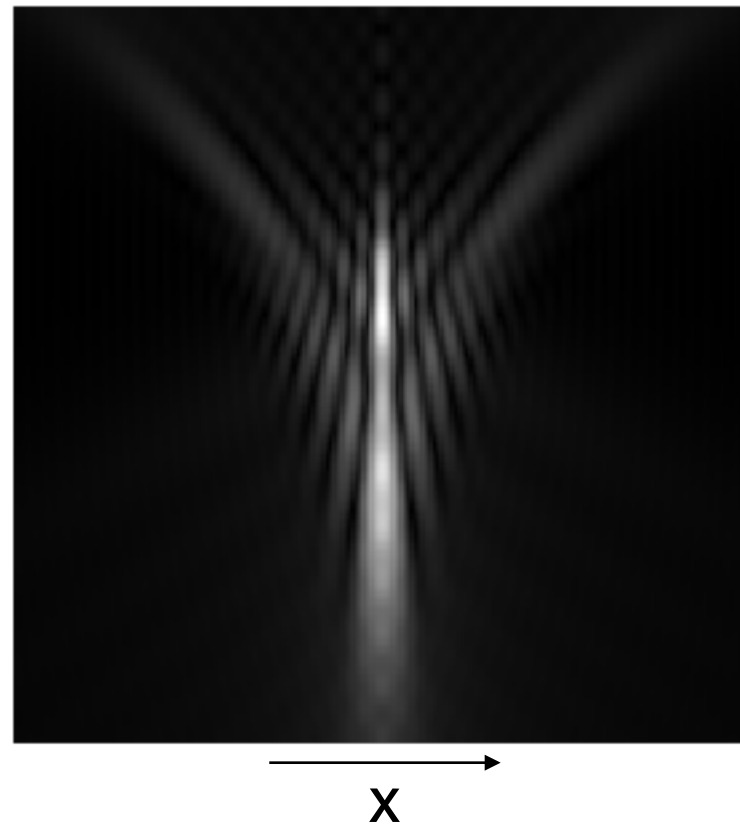
Spherical Aberration

Point spread functions

Ideal



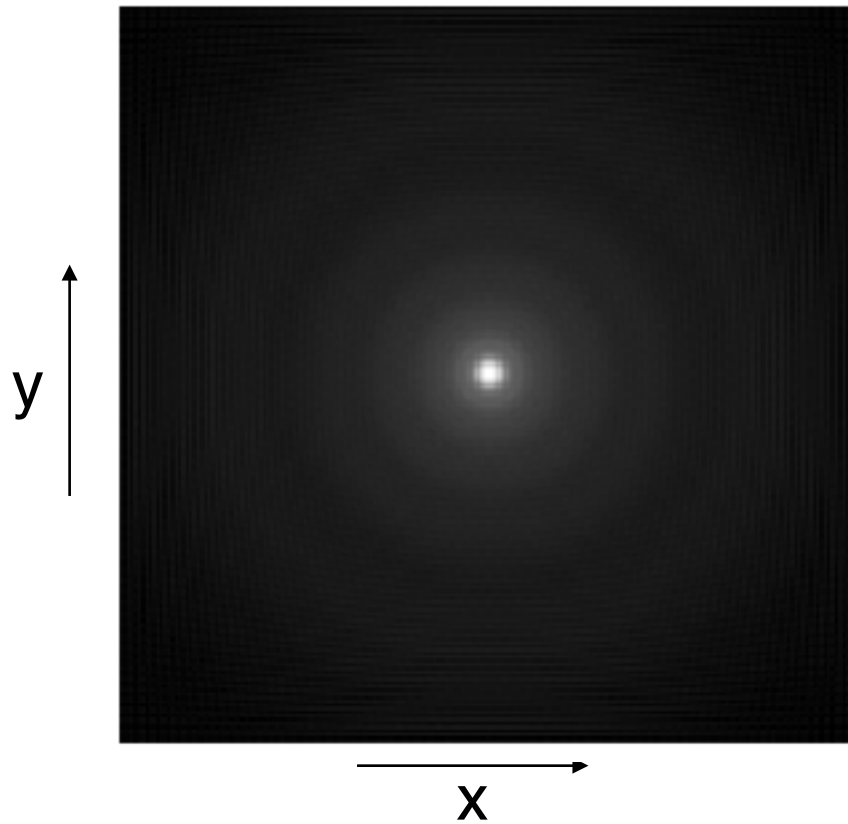
1 wave of spherical ab



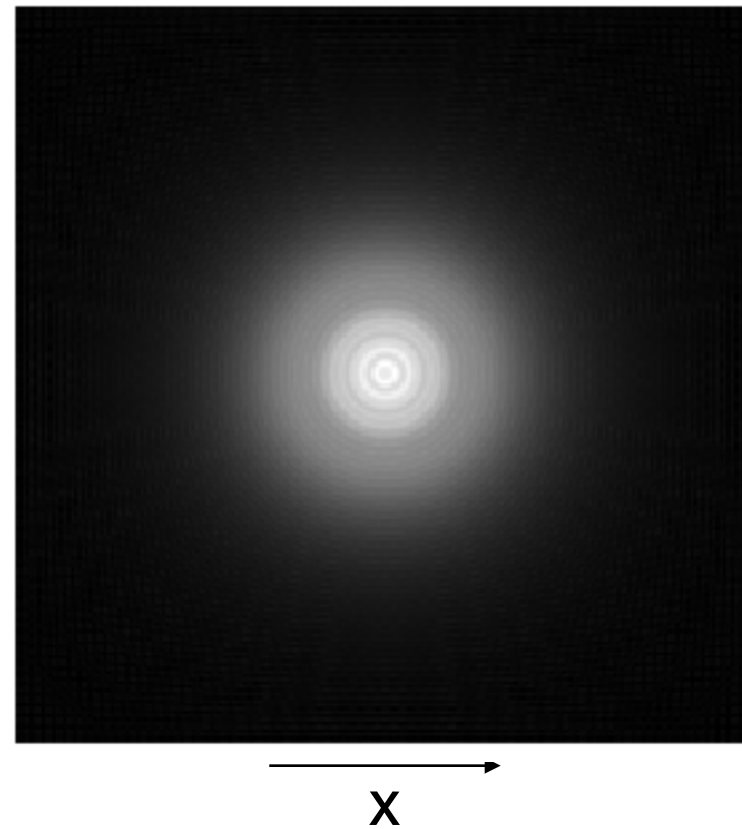
Spherical Aberration

Point spread functions

Ideal



1 wave of spherical ab



Sources of Spherical Aberration

Design compromises

Manufacturing tolerances

Immersion fluid index error

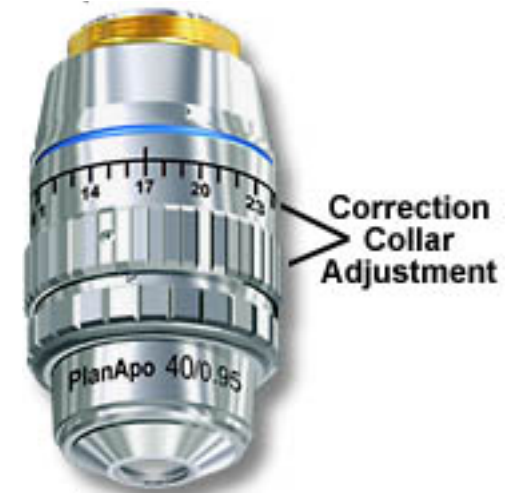
Temperature variation

Cover slip thickness

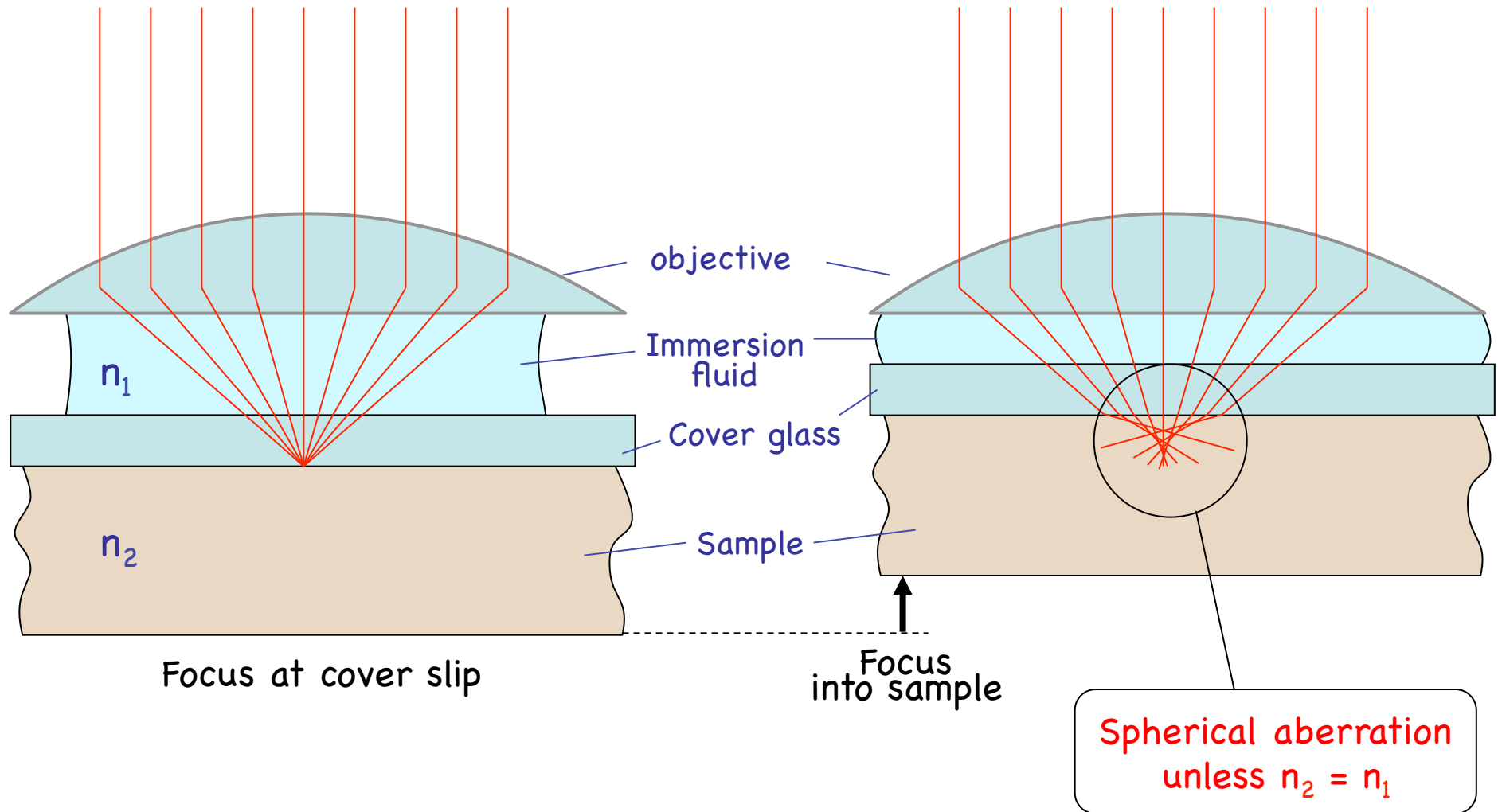
(high-NA objectives except oil immersion)

Correction collar setting

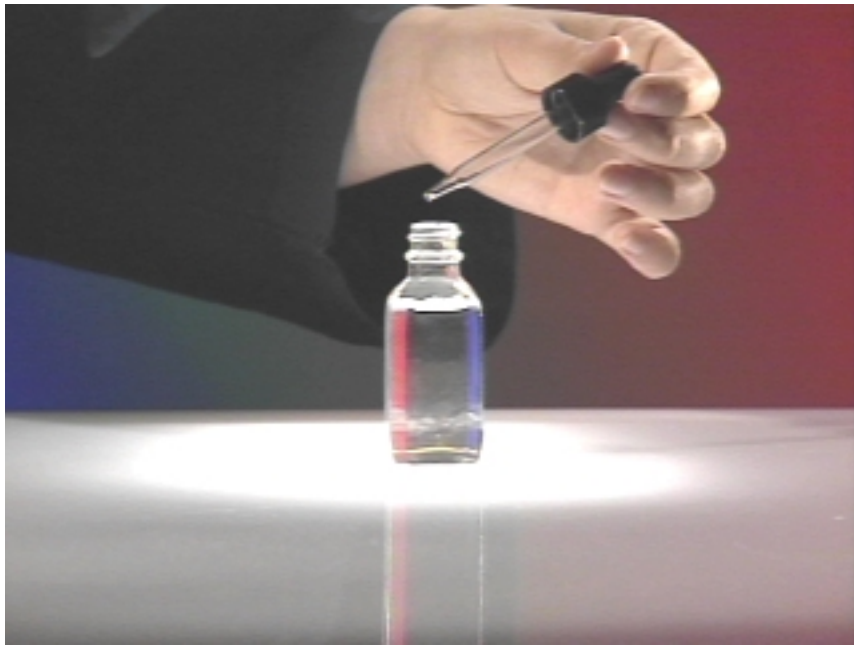
Sample refractive index mismatch



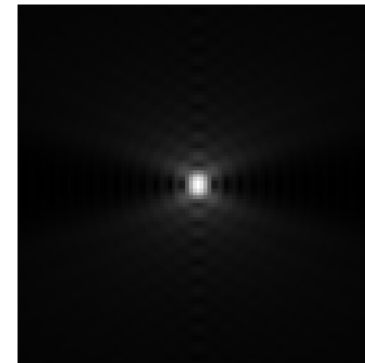
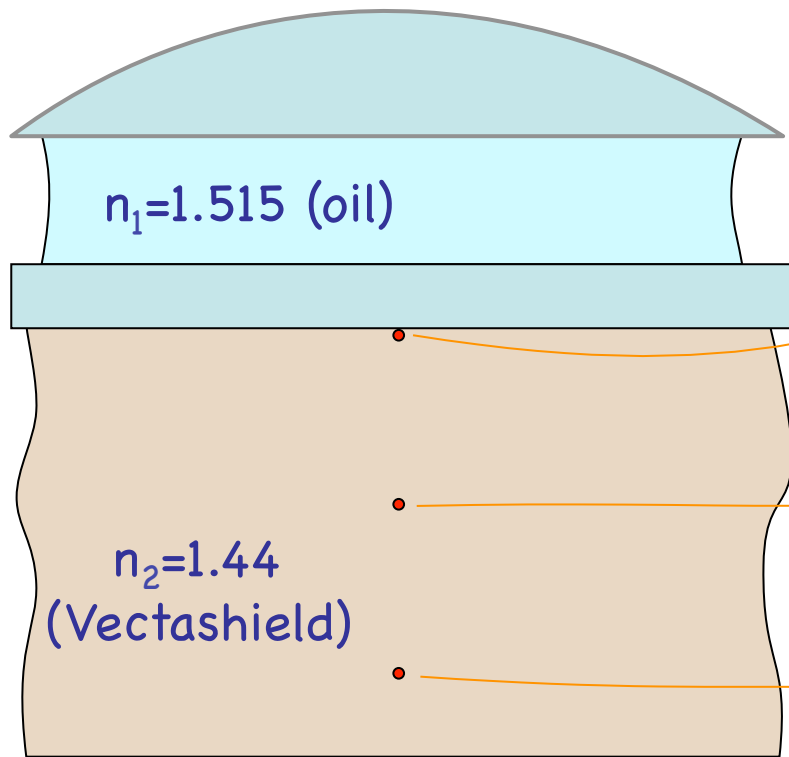
Index Mismatch & Spherical Aberration



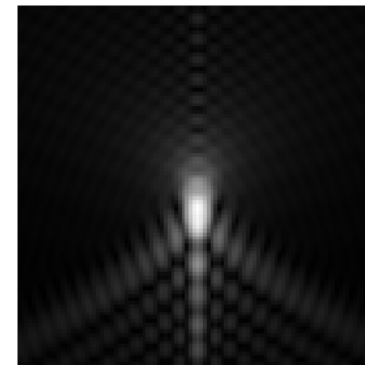
Index matching



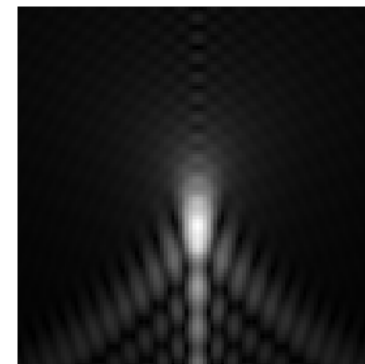
Index Mismatch & Spherical Aberration



$z=0 \mu\text{m}$

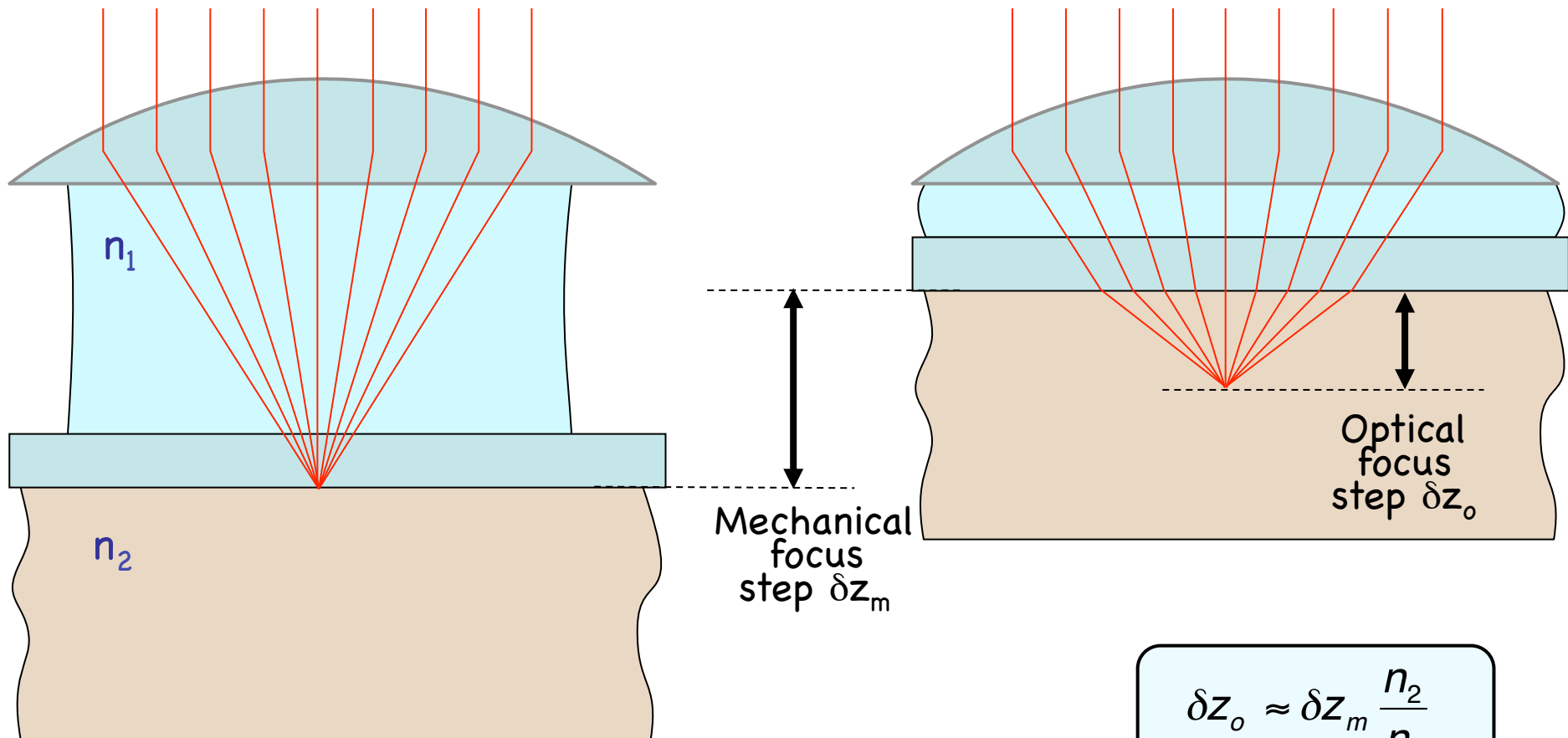


$z=25 \mu\text{m}$



$z=50 \mu\text{m}$

Index Mismatch & Axial Scaling

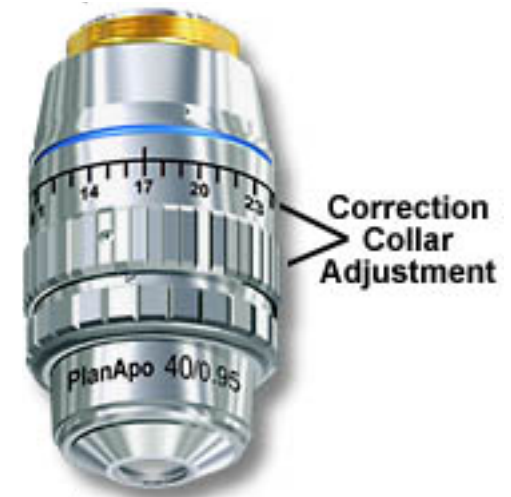


$$\delta z_o \approx \delta z_m \frac{n_2}{n_1}$$

If there is index mismatch,
your z pixel size is not what you think

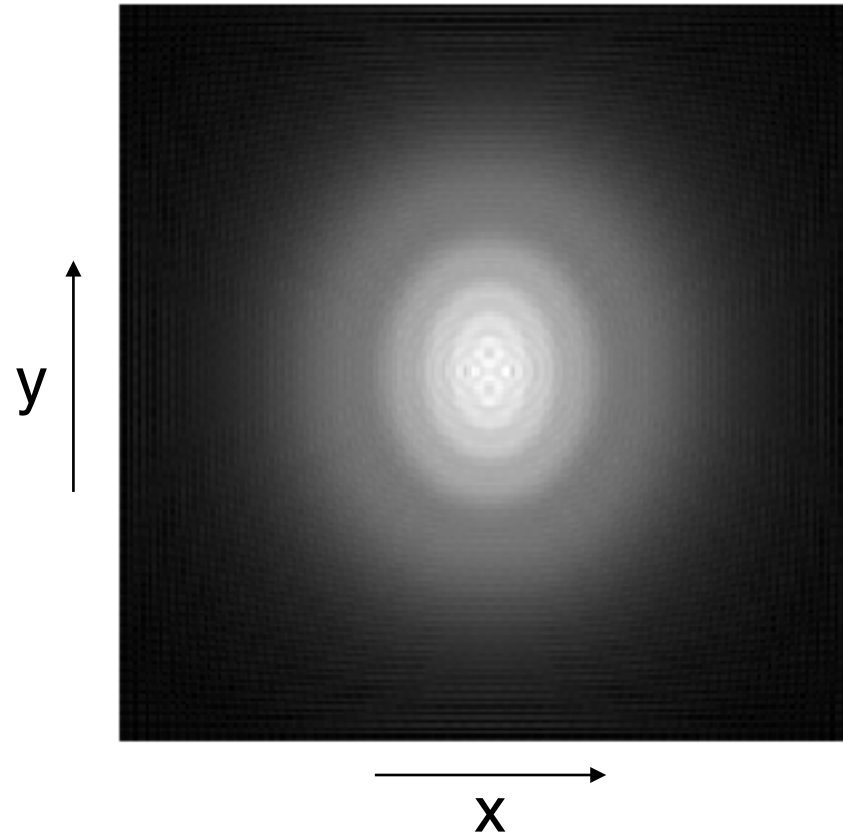
Getting Rid of Spherical Aberration

- Use correct and consistent cover slips
- Pick a room with stable temperature $\approx 20^{\circ}\text{C}$
- Use special immersion iof for 37°C live work
- Adjust correction collar
- If no collar, adjust immersion medium index
- **Use an objective that is matched to the mounting medium:**
 - For aqueous samples, use a water immersion objective
 - For fixed samples viewed with oil immersion objectives, ideally use a mounting medium with index ≈ 1.515
 - For fixed samples in commercial media, ideally use a glycerol immersion objective



Astigmatism

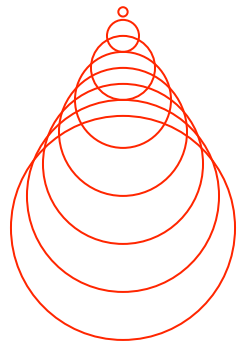
Point spread function



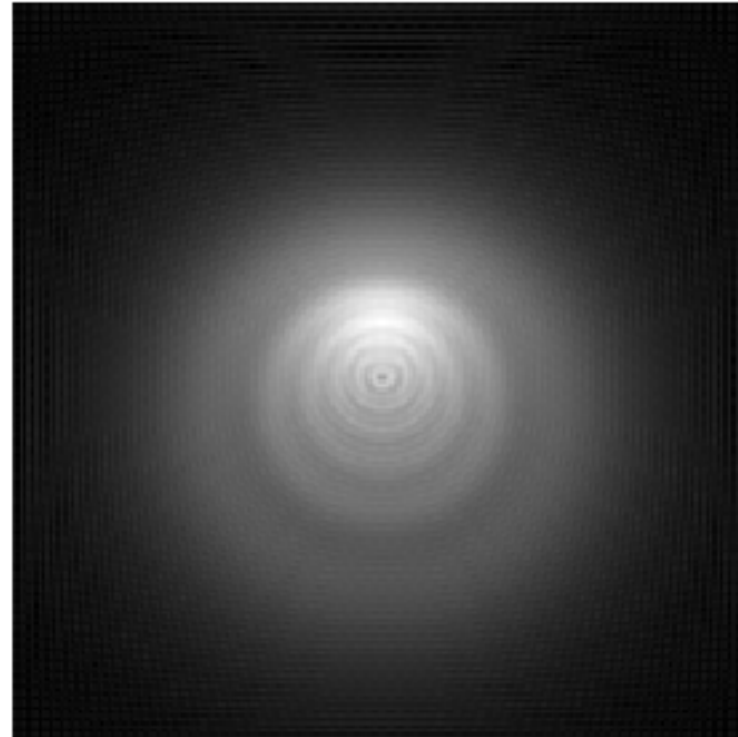
1 wave p-p of
x-y astigmatism

Coma

Point spread function



y



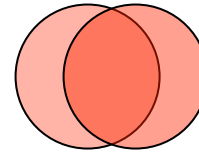
x

1 wave p-p of
y coma

Sources of Astigmatism & Coma

Off-axis (edges of field of view)

- All objectives have some vignetting
- Present in the design
- You get what you pay for

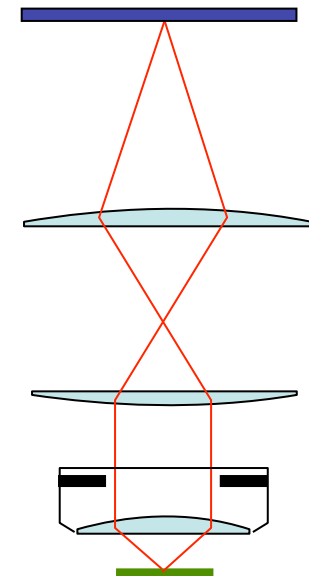
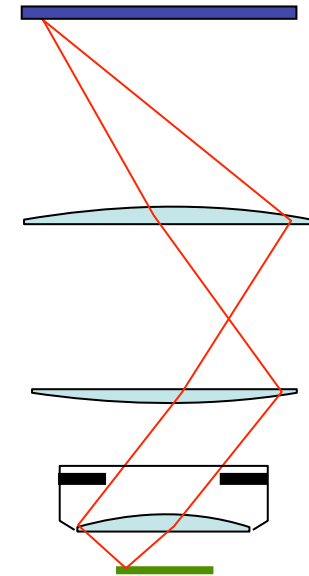


On-axis (center of field of view)

Should be none, by symmetry.

If they are there, they could be from:

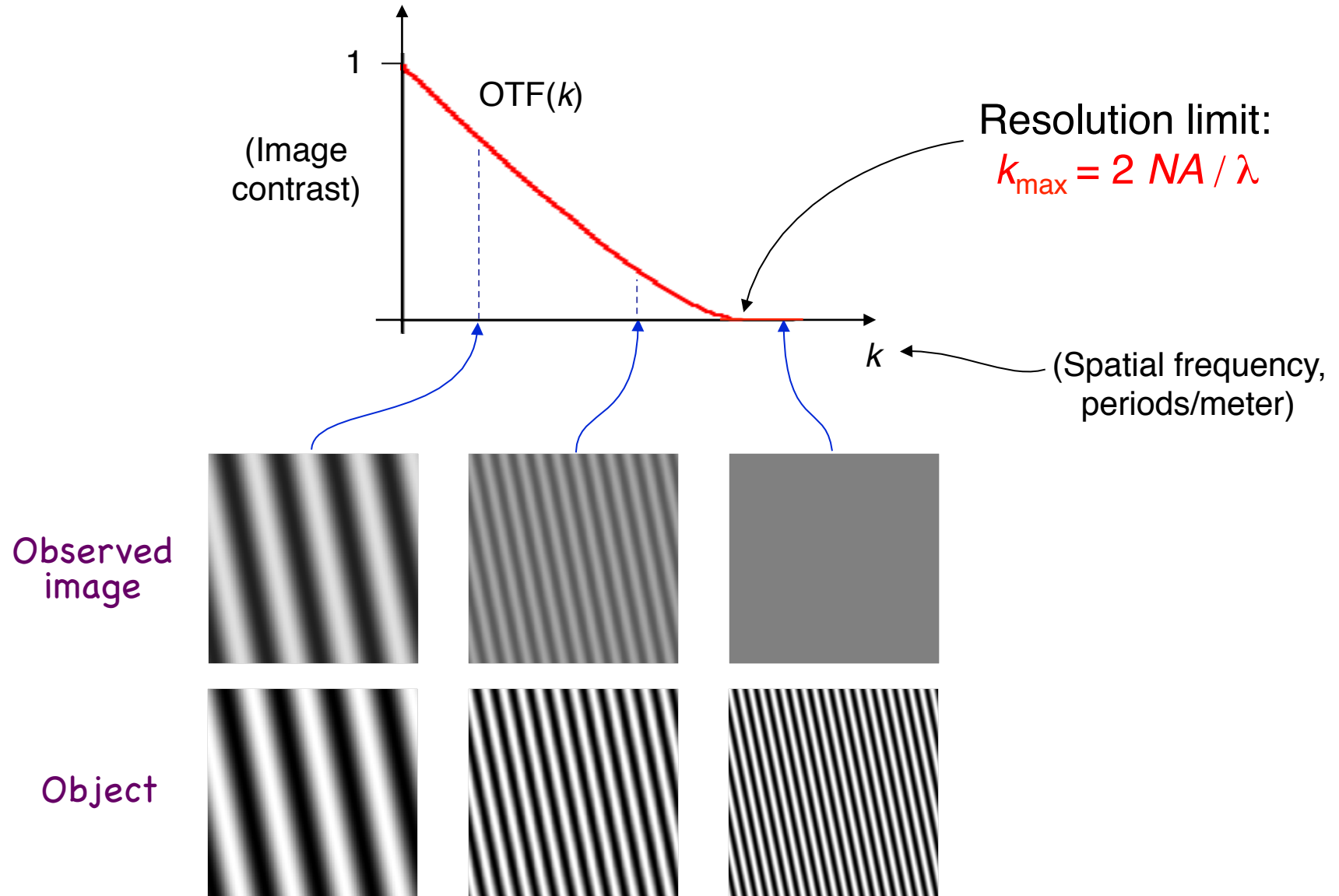
- manufacturing or assembly tolerances
- dirt or abuse
- Misalignment (tilt, off-axis shift of something)
- bad downstream components (mirrors, dichroics, filters...)
- **Air bubble** in the immersion fluid or sample
- **Tilted cover slip**
(dry and water-immersion high-NA lenses)



More about Spatial frequencies & the Optical Transfer Function (OTF)

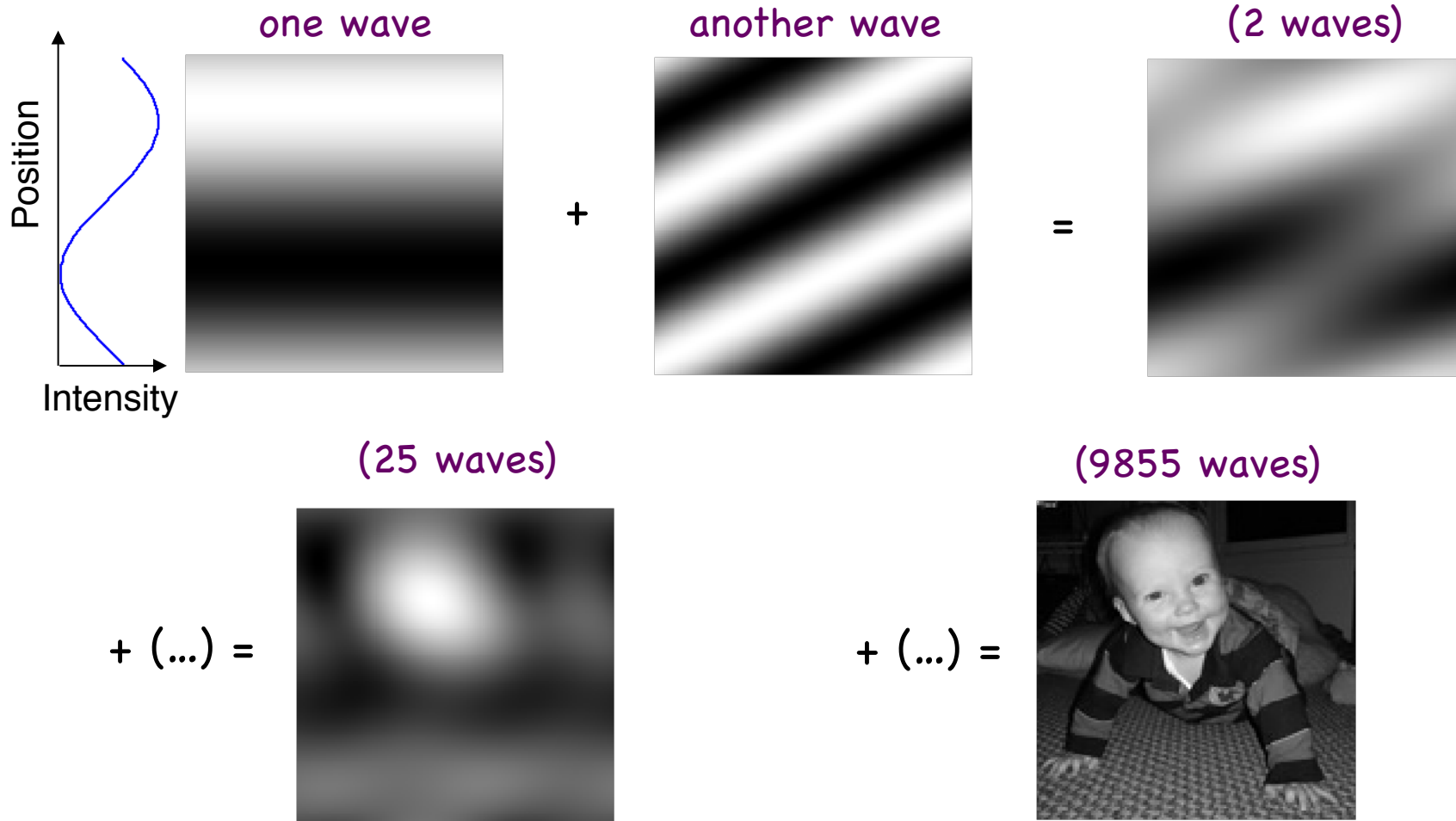
For the record only, not for this course
Attribute to Mats Gustafsson

The response to pure waves is well-defined by the Optical Transfer Function (OTF)



Think of Images as Sums of Waves

... or “spatial frequency components”

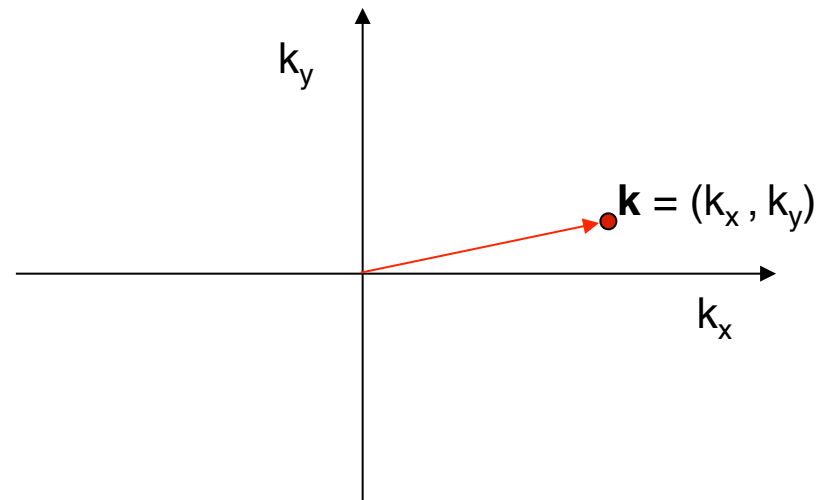
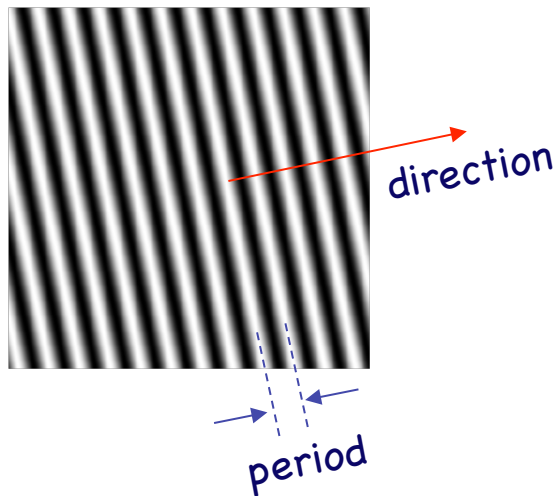


Frequency Space

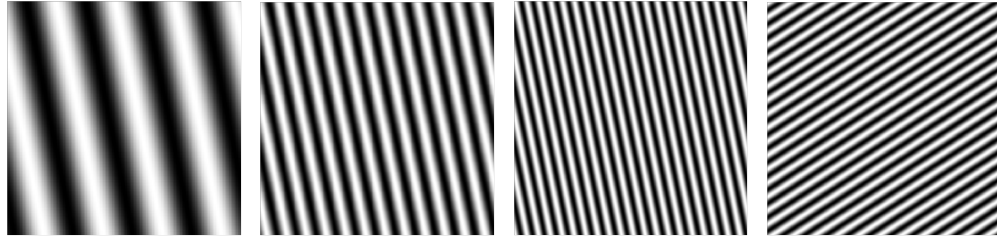
To *describe* a wave,
we need to specify its:

- Frequency (how many periods/meter?) → Distance from origin
 - Direction → Direction from origin
 - Amplitude (how strong is it?) → Magnitude of value
 - Phase (where are the peaks & troughs?) → Phase of value
- (complex)

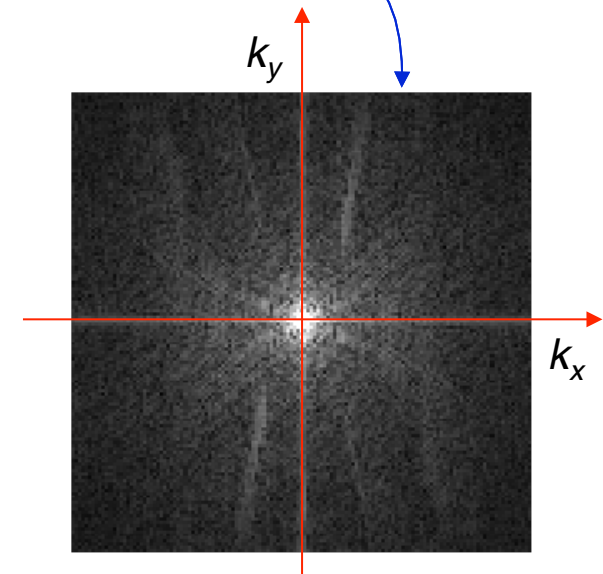
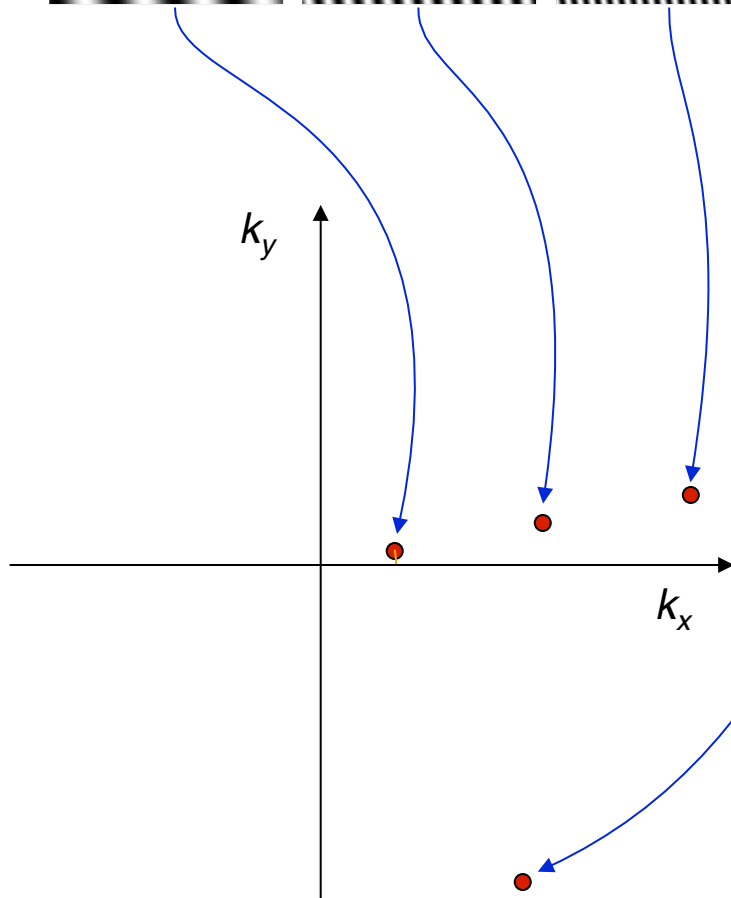
Can describe it by
a *value at a point*



Frequency Space and the *Fourier Transform*



Fourier Transform



Properties of the Fourier Transform

$$F(\mathbf{k}) = \int f(\mathbf{r})e^{2\pi i\mathbf{k}\cdot\mathbf{r}} d\mathbf{r}$$

Completeness:

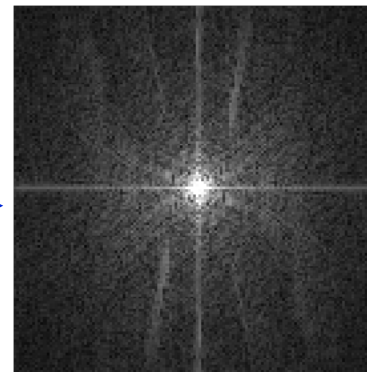
The Fourier Transform contains **all** the information of the original image

Symmetry:

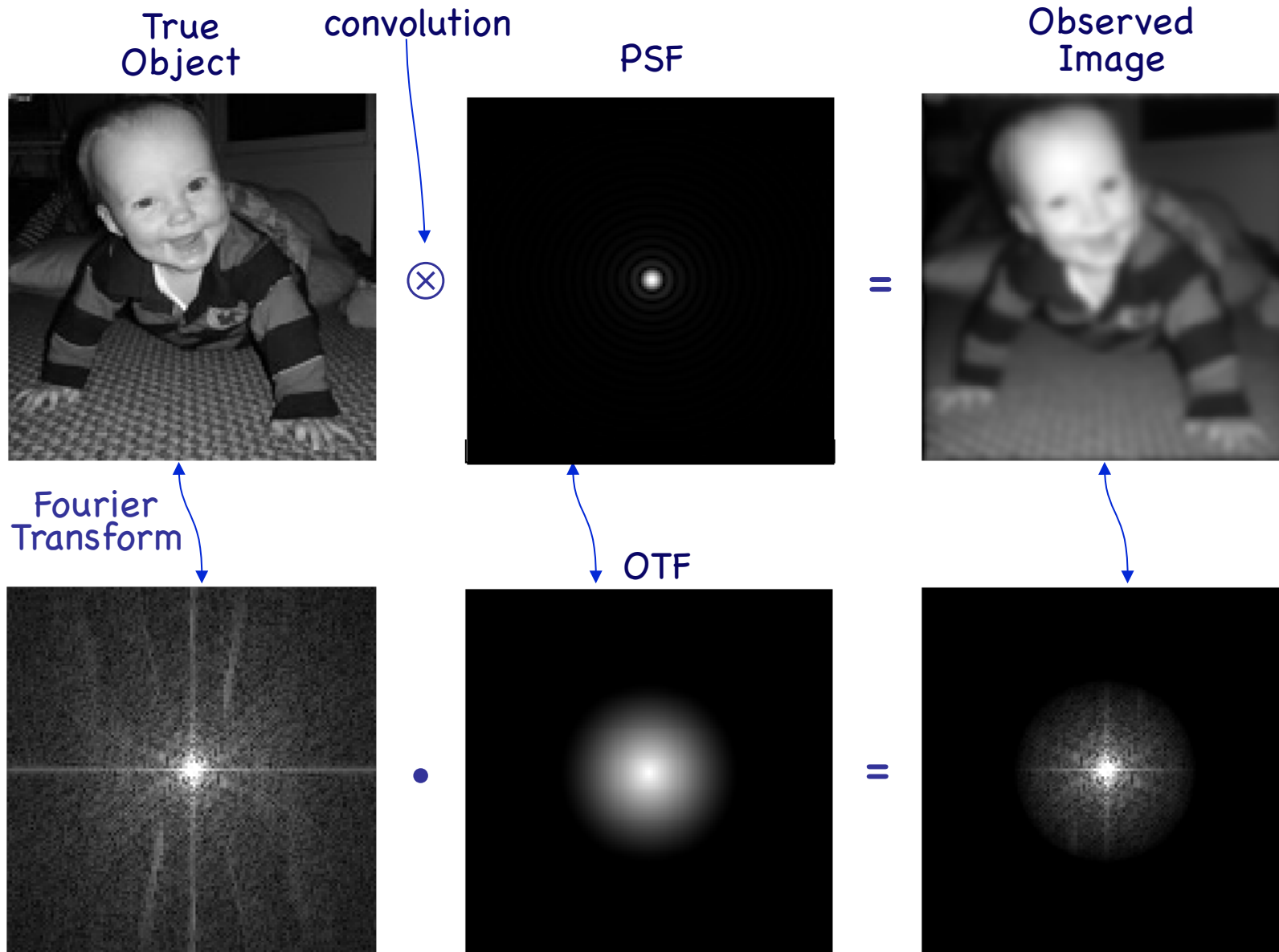
The Fourier Transform of the Fourier Transform is the original image



Fourier transform



The OTF and the PSF are Fourier transforms of each other



Convolutions

$$(f \otimes g)(r) = \int f(a) g(r-a) da$$

Why do we care?

- They are everywhere...
- The convolution theorem:

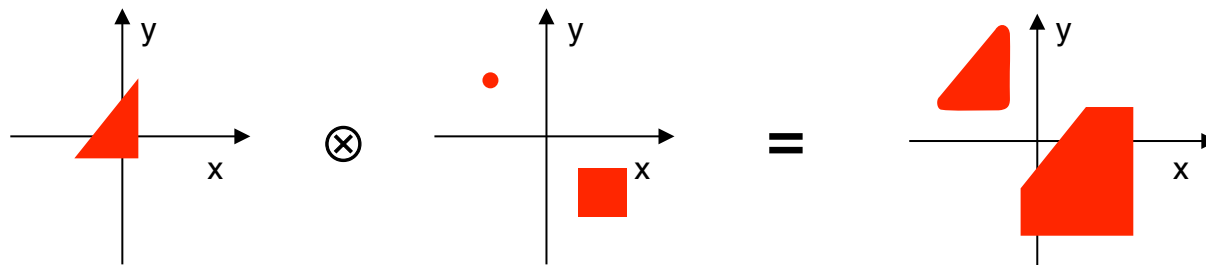
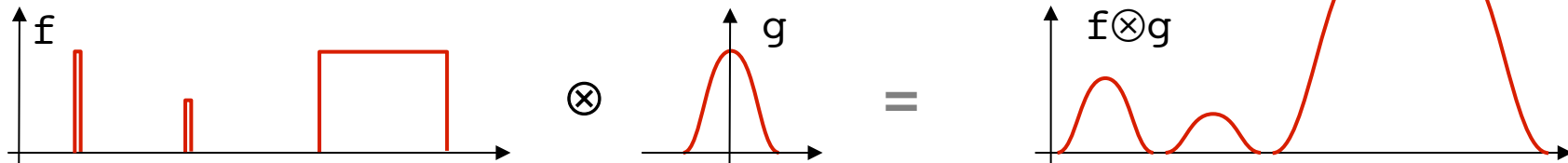
If $h(r) = (f \otimes g)(r)$,
 then $\tilde{h}(k) = \tilde{f}(k) \tilde{g}(k)$

A convolution in real space becomes a product in frequency space & vice versa

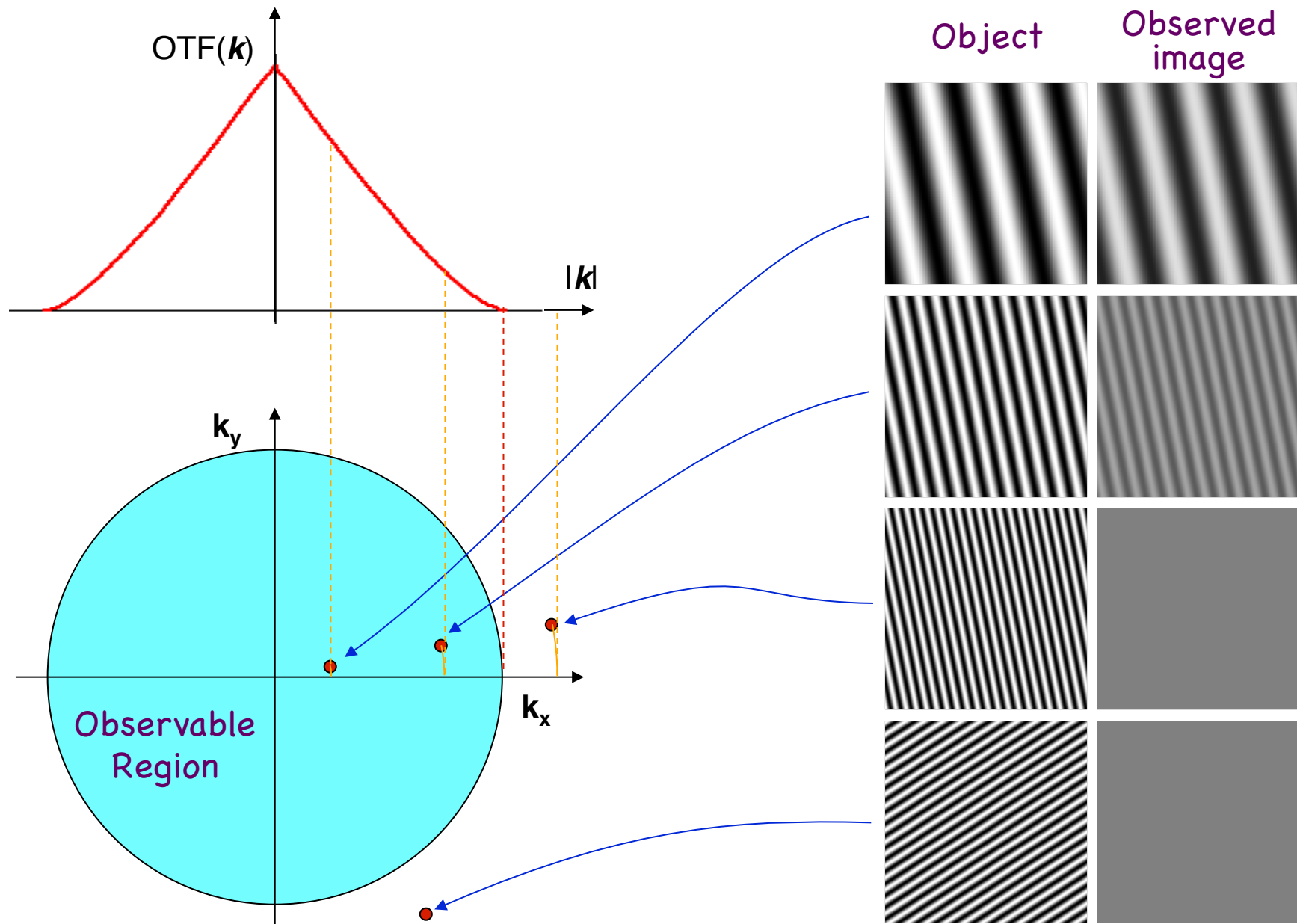
Symmetry: $g \otimes f = f \otimes g$

So what is a convolution, intuitively?

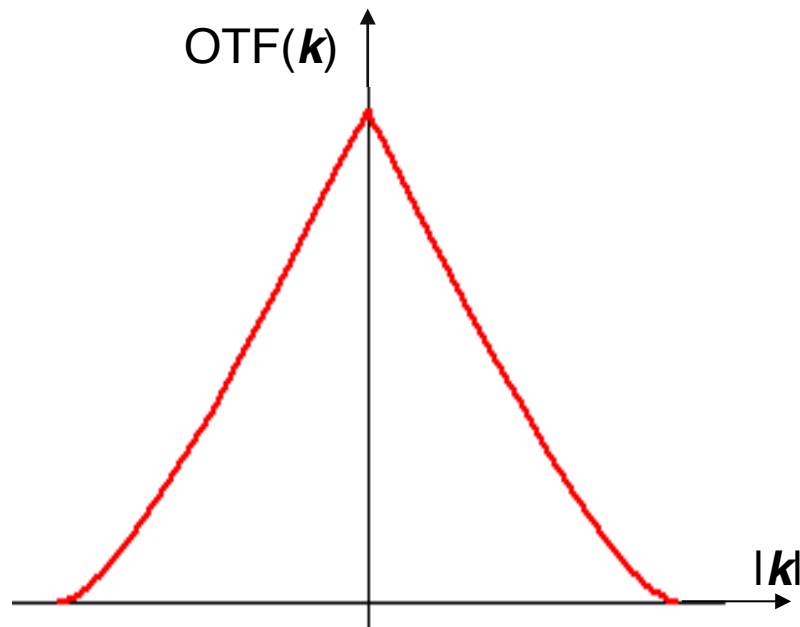
- “Blurring”
- “Drag and stamp”



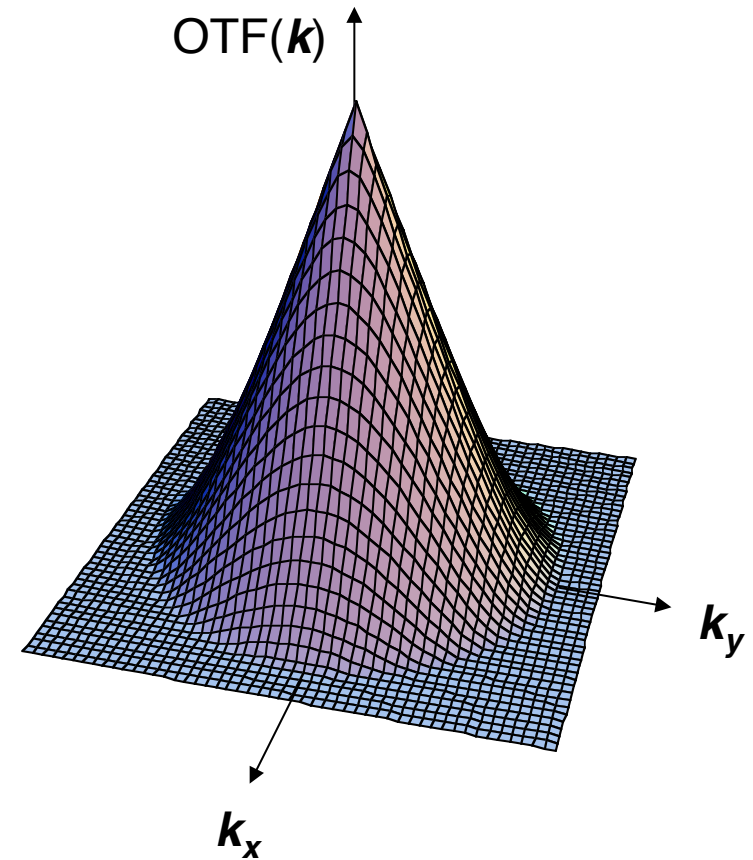
The Transfer Function Lives in Frequency Space



The 2D In-focus Optical Transfer Function (OTF)

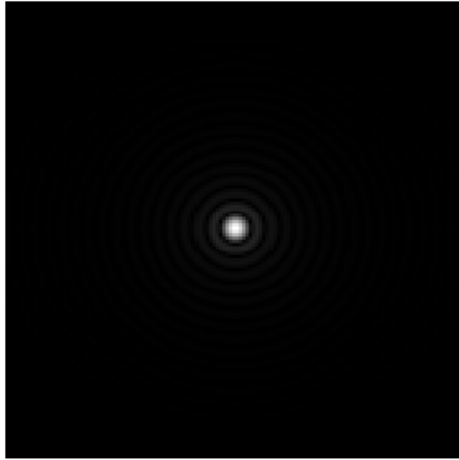


(Idealized
calculations)



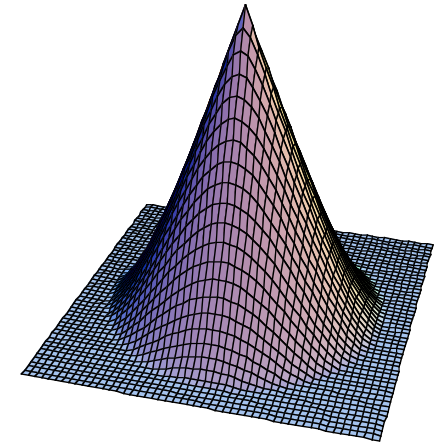
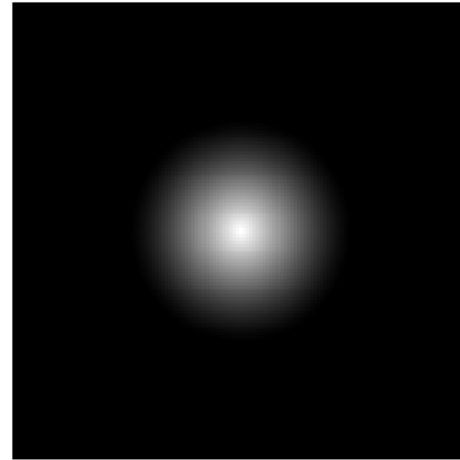
The 3D OTF

2D PSF

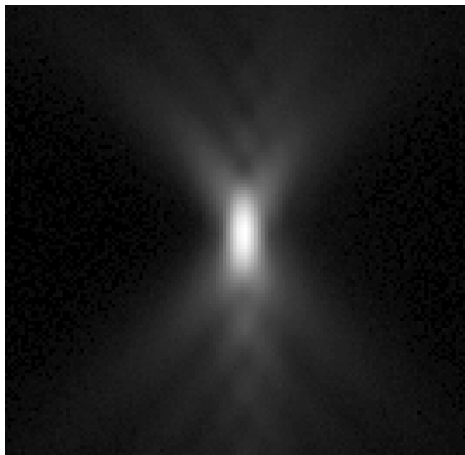


2D F.T.
↔

2D OTF

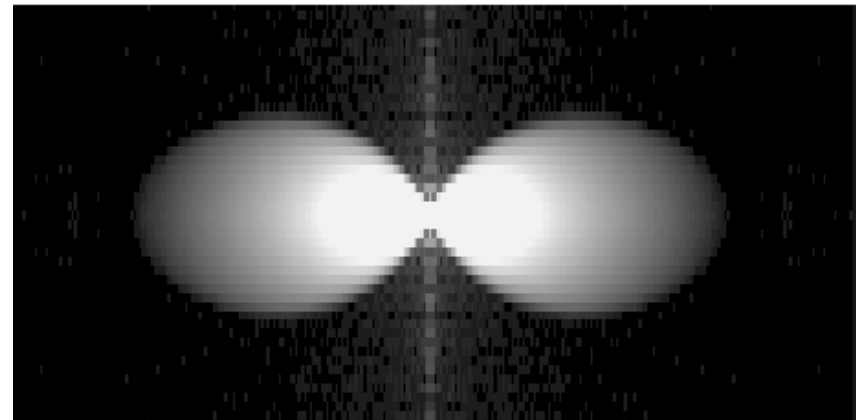


3D PSF

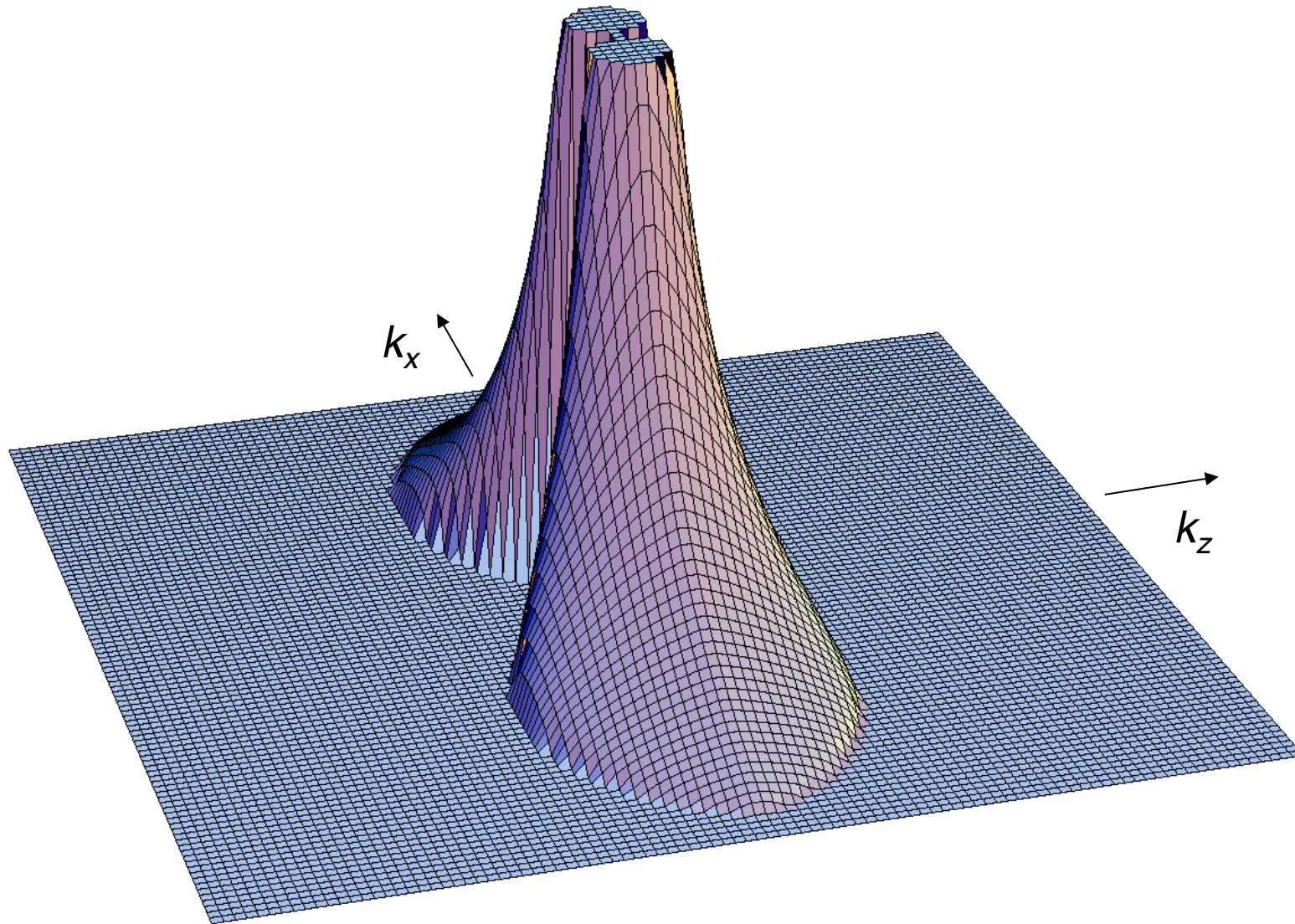


3D F.T.
↔

3D OTF



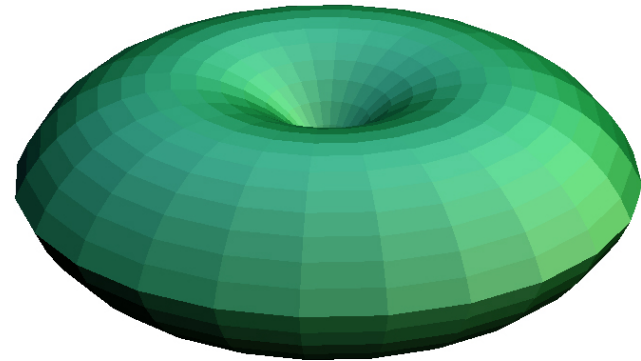
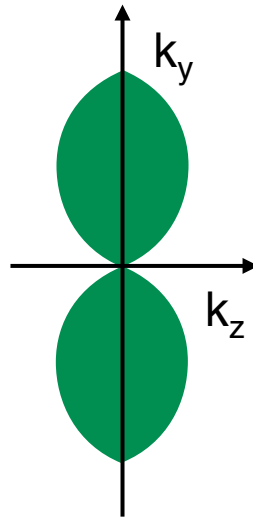
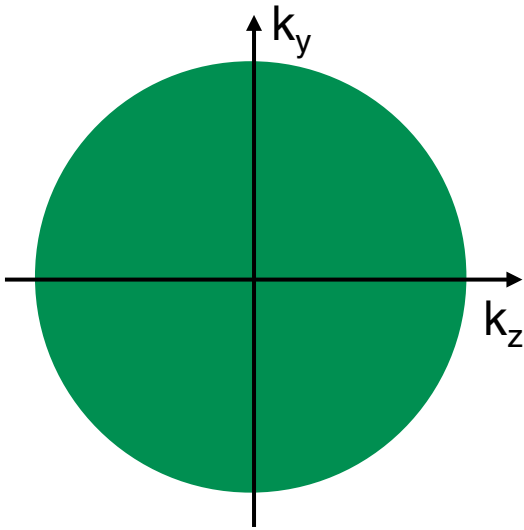
Values of the 3D OTF



3D Observable Region

= OTF support

= Region where the OTF is non-zero



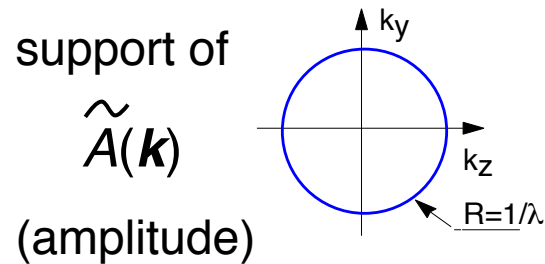
Why this weird region?

Monochromatic light

In free space

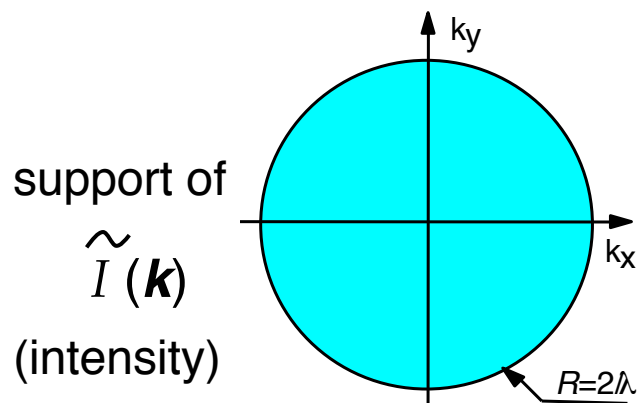


Monochromatic light has only one wavelength $\lambda \rightarrow$ only one $|k| = 1 / \lambda$



\rightarrow The light amplitude $A(\mathbf{i})$ has Fourier components only on a shell of radius $1 / \lambda$

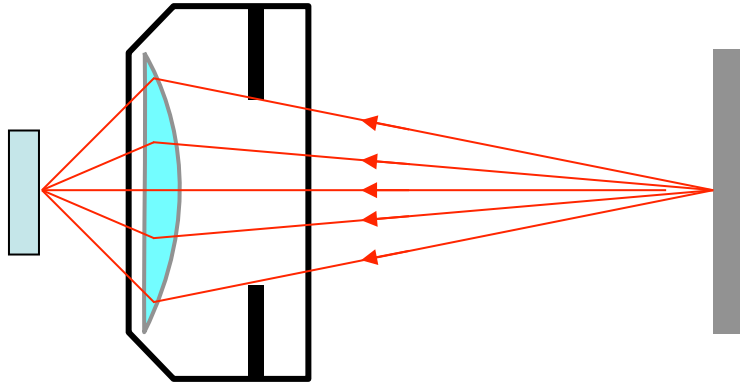
The intensity $I(\mathbf{r}) = |A(\mathbf{r})|^2$



In reciprocal space, this product A^*A becomes a convolution $\tilde{A} \otimes \tilde{A}$ of the shell with itself, which is a sphere of twice the radius

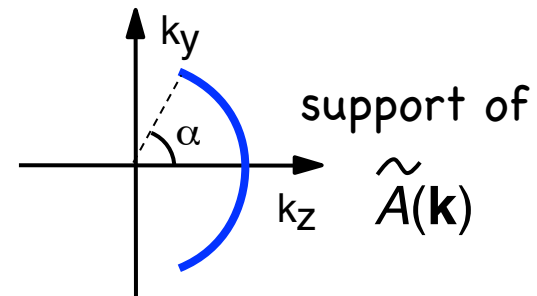
This sphere indicates all frequency components of the light intensity that can ever be non-zero

Consider light from a camera pixel into the sample.
What are the Fourier components of this light?

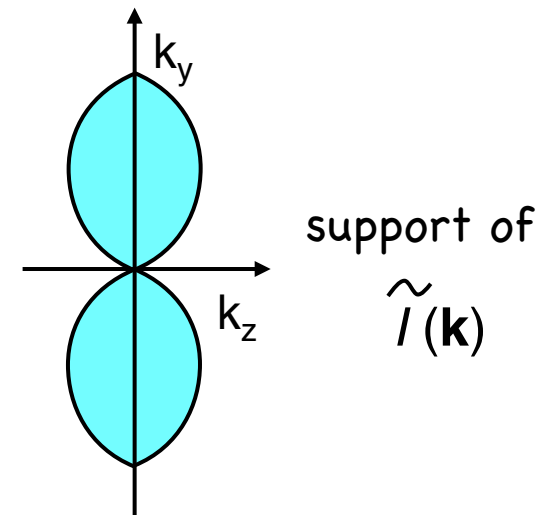


Light enters the sample only from those directions allowed by the aperture angle α

Only a bowl-shaped segment of the shell makes it through the objective:

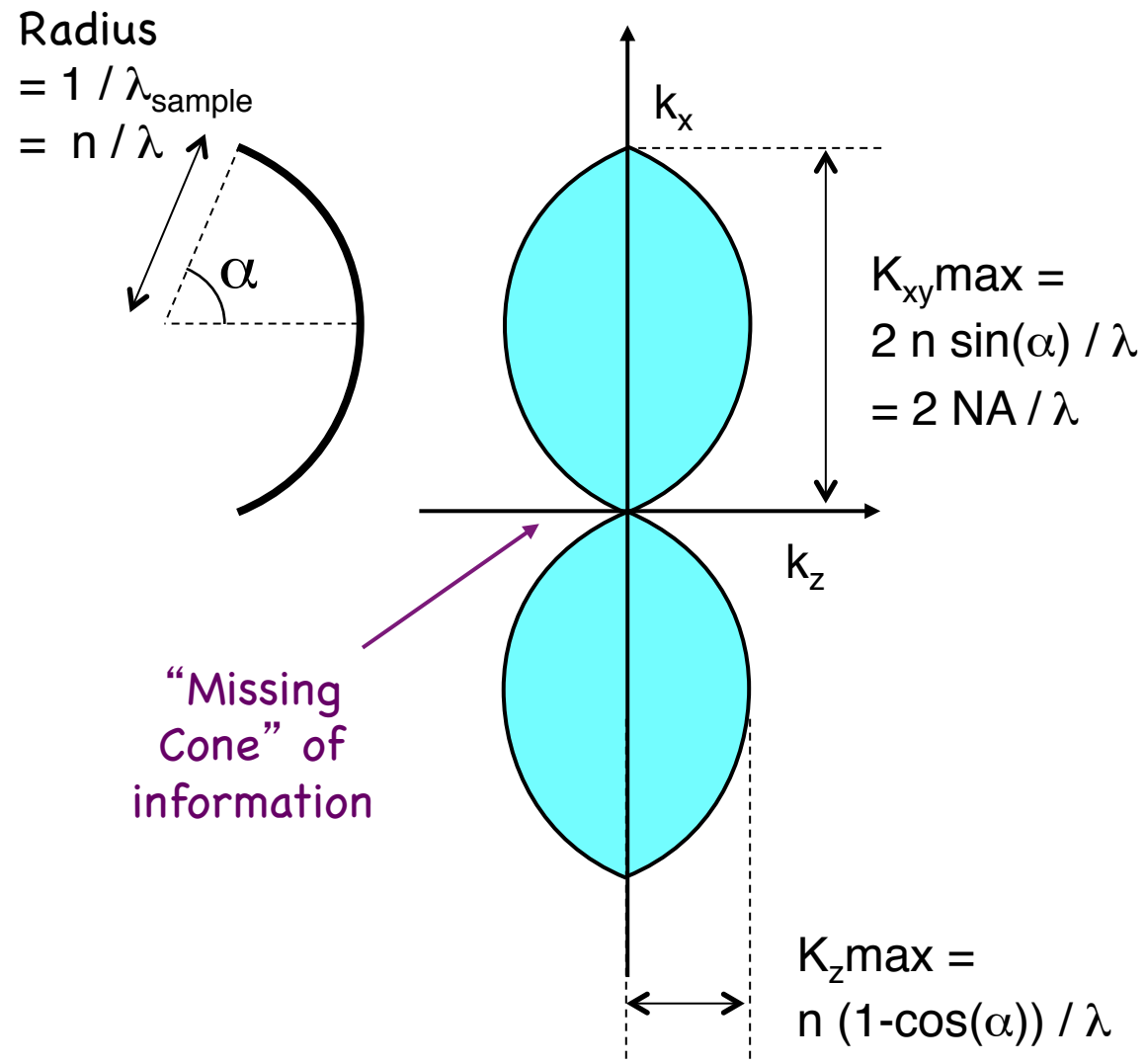


The intensity now becomes a convolution of the **bowl** with itself, which has a donut-shaped region of support.

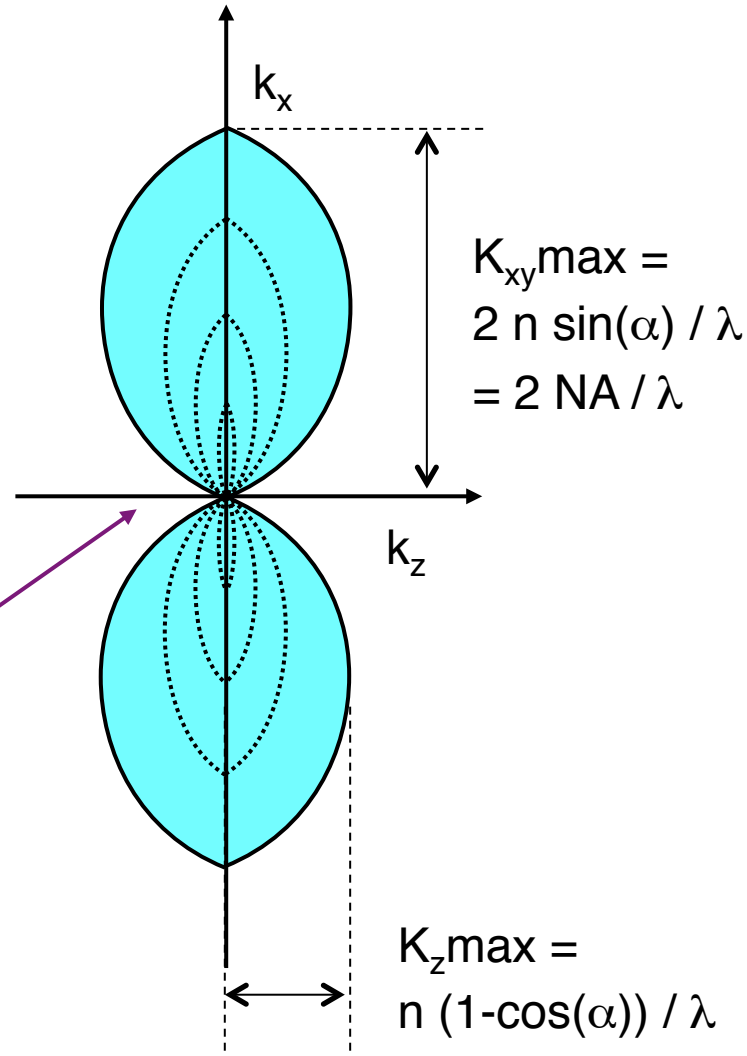
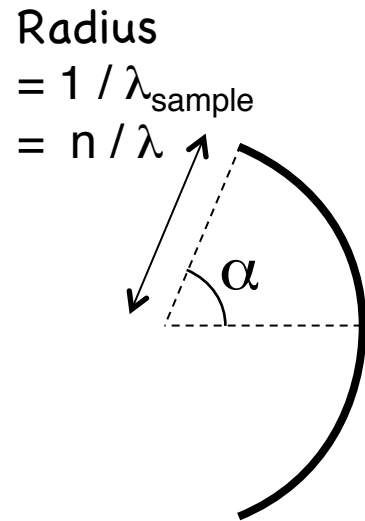


This is the **OTF support**:
the set of sample frequencies that can be detected through the microscope

So what is the resolution?



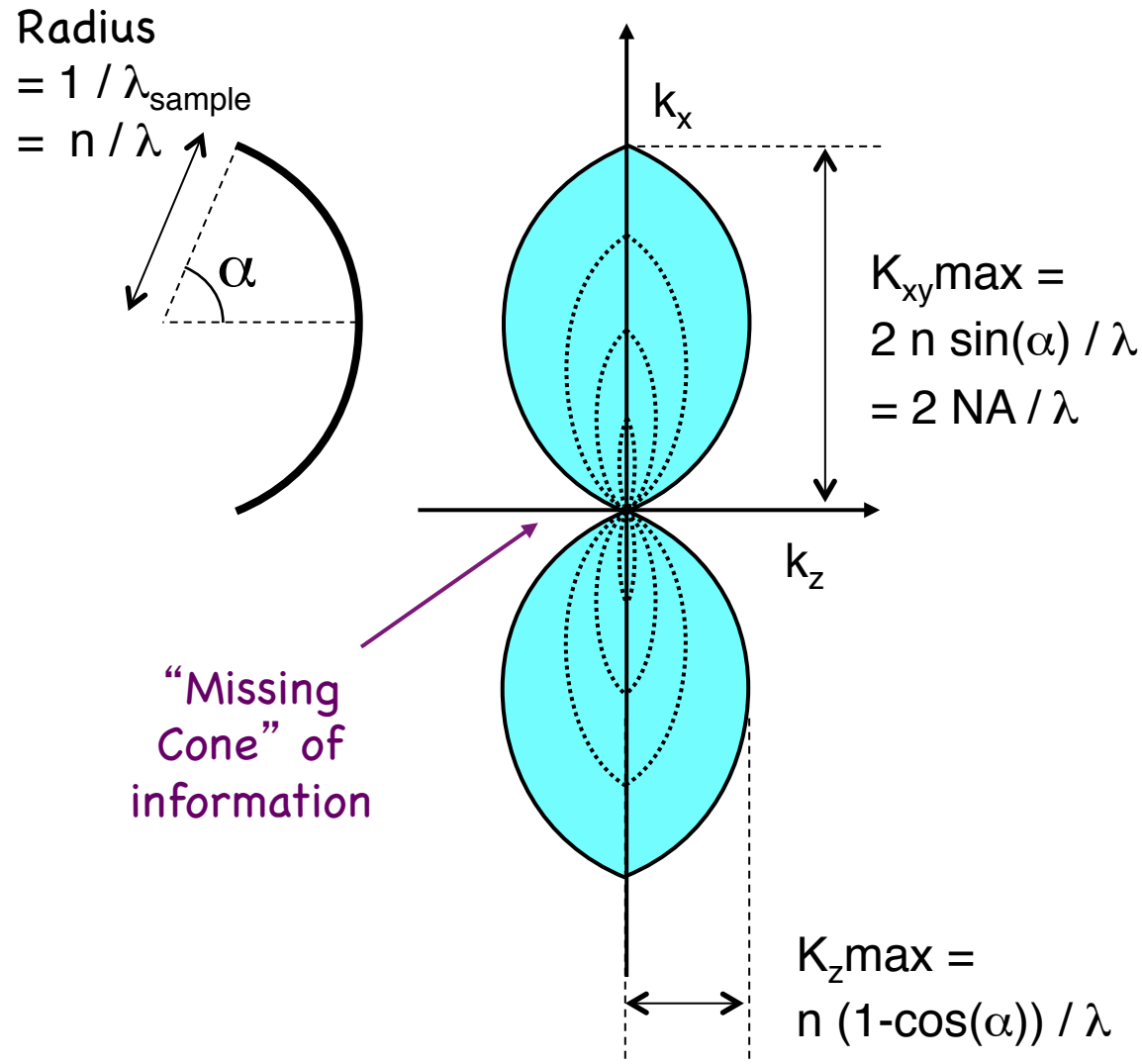
So what is the resolution?



Lowering the NA
Degrades the
axial resolution
faster than the
lateral resolution

But low axial resolution
= long *depth of field*
This is *good*,
if 2D is enough

So what is the resolution?



Example:
a high-end objective

$$\text{NA} = 1.4$$

$$n = 1.515$$

$$\rightarrow \alpha = 67.5^\circ$$

$$\lambda = 600 \text{ nm}$$



Lateral (XY) resolution:

$$1 / K_{xy, \text{max}} = \mathbf{0.21 \mu m}$$

Axial (Z) resolution:

$$1 / K_{z, \text{max}} = \mathbf{0.64 \mu m}$$

Nomenclature

- Optical Transfer Function, OTF
Complex value with amplitude and phase
- Contrast Transfer Function, CTF
- Modulation Transfer Function, MTF
Same thing without the phase information